

Molecular imaging of tau in the pathological cascade of Alzheimer's disease



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Molecular imaging of tau in the pathological cascade of Alzheimer's disease

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This thesis is dedicated to the patients and their relatives.

*Οὐ γὰρ ὡς ἀγγεῖον ὁ νοῦς ἀποπληρώσεως ἀλλ’
ὑπεκκαύματος μόνον ὥσπερ ὕλη δεῖται, ὁρμὴν
ἐμποιοῦντος εὐρετικὴν καὶ ὄρεζιν ἐπὶ τὴν ἀλήθειαν.*

— Πλούταρχος, *Περὶ τοῦ ἀκούειν*

*For the correct analogy for the mind is not a vessel
that needs filling, but wood that needs igniting –
no more – and then it motivates one towards
originality and instils the desire for truth.*

— Plutarch, *On listening*

ABSTRACT

The pathology of Alzheimer's disease (AD) is characterised by the misfolding and aggregation of amyloid- β (A β) into extracellular plaques and aggregation of tau into intracellular neurofibrillary tangles. Recent advances in molecular imaging have allowed the development of positron emission tomography (PET) tracers for the *in vivo* detection of A β plaques while current efforts focus on the evaluation of recently proposed tracers targeting tau pathology. This thesis is composed of three main parts. Part one compares two A β PET tracers ([^{11}C]PIB and [^{18}F]florbetapir) when administered to different but matched patient cohorts, and explores the effect of age on the distribution of A β -positive PET scans. Part two focuses on the first *in vivo* evaluation of the tau-specific tracer [^{18}F]THK5317, using a longitudinal multi-modal design, in a sample of cognitively normal volunteers, patients at different clinical stages of AD and individual patients with atypical parkinsonism. The third part describes the direct *in vivo* comparison of the binding properties of two tau-specific tracers ([^{11}C]THK5351 and [^{11}C]PBB3) when injected into the same patients with AD on the same day. The results indicated that, firstly, the binding of the A β -specific PET tracers, [^{11}C]PIB and [^{18}F]florbetapir, was highly comparable in individuals from different cohorts. Furthermore, age plays an important role in the distribution of A β -positive PET scans, with the oldest old patients with cognitive complaints appearing to benefit substantially from clinical assessment with A β PET. Secondly, the tracer [^{18}F]THK5317 detected the expected load and regional distribution of tau pathology *in vivo* in a sample of patients with AD and patients with atypical parkinsonism. The distribution of [^{18}F]THK5317 binding differed from that of A β deposition in patients with AD, although regional correlations existed, indicating areas where A β and tau pathologies were co-located. The regional load of tau pathology ([^{18}F]THK5317) was associated with measures of global cognition and episodic memory, with local hypometabolism playing a mediating role in this relationship. Longitudinally, a heterogeneous pattern of changes was observed in the binding of the tau tracer [^{18}F]THK5317 in patients with AD, in contrast to the homogeneous changes in glucose metabolism that better tracked cognitive deterioration. The build-up of tau pathology ([^{18}F]THK5317) and the development of local hypometabolism appeared temporally dissociated, with a stronger relationship detected between the two when hypometabolism changes became more prevalent, in the later stages of the disease. Finally, different tau-specific tracers ([^{11}C]THK5351 and [^{11}C]PBB3) seemed to bind *in vivo* to different molecular targets; [^{11}C]PBB3 binding appeared to correlate closer to A β deposition, while [^{11}C]THK5351 binding followed the expected regional pattern of tau pathology in AD and related closer to downstream markers of the disease. Further investigation of the existing PET tracers and development of new tracers is required for shedding light on the pathological processes that contribute to neurodegeneration in AD and for developing clinical markers that allow early and highly accurate discrimination between different proteinopathies.

LIST OF PUBLICATIONS

The thesis is based on the following original articles.

- I. **Chiotis K**, Carter SF, Farid K, Savitcheva I, Nordberg A; Diagnostic Molecular Imaging (DiMI) network and the Alzheimer's Disease Neuroimaging Initiative. Amyloid PET in European and North American cohorts; and exploring age as a limit to clinical use of amyloid imaging.
Eur J Nucl Med Mol Imaging. 2015 Sep;42(10):1492-506.
- II. **Chiotis K**, Saint-Aubert L, Savitcheva I, Jelic V, Andersen P, Jonasson M, Eriksson J, Lubberink M, Almkvist O, Wall A, Antoni G, Nordberg A. Imaging *in vivo* tau pathology in Alzheimer's disease with THK5317 PET in a multimodal paradigm.
Eur J Nucl Med Mol Imaging. 2016 Aug;43(9):1686-99.
- III. Saint-Aubert L, Almkvist O, **Chiotis K**, Almeida R, Wall A, Nordberg A. Regional tau deposition measured by [¹⁸F]THK5317 positron emission tomography is associated to cognition via glucose metabolism in Alzheimer's disease.
Alzheimers Res Ther. 2016;8(1):38.
- IV. **Chiotis K**, Saint-Aubert L, Rodriguez-Vieitez E, Leuzy A, Almkvist O, Savitcheva I, Jonasson M, Lubberink M, Wall A, Antoni G, Nordberg A. Longitudinal changes of tau PET imaging in relation to hypometabolism in prodromal and Alzheimer's disease dementia.
Mol Psychiatry. 2017; Epub 2017 May 16.
- V. **Chiotis K**, Stenkrona P, Almkvist O, Stepanov V, Ferreira D, Arakawa R, Takano A, Westman E, Varrone A, Okamura N, Shimada H, Higuchi M, Halldin C, Nordberg A. Dual tracer tau PET imaging reveals different molecular targets for ¹¹C-THK5351 and ¹¹C-PBB3 in the Alzheimer brain.
Manuscript in preparation.

SELECTION OF RELATED PUBLICATIONS

This is an excerpt of related publications by the author, containing supporting evidence, or revising the existing literature.

Original articles

Rodriguez-Vieitez E, Leuzy A, **Chiotis K**, Saint-Aubert L, Wall A, Nordberg A. Comparability of [^{18}F]THK5317 and [^{11}C]PIB blood flow proxy images with [^{18}F]FDG positron emission tomography in Alzheimer's disease. *J Cereb Blood Flow Metab.* 2017;37(2):740-749.

Jonasson M, Wall A, **Chiotis K**, Saint-Aubert L, Wilking H, Sprycha M, Borg B, Thibblin A, Eriksson J, Sörensen J, Antoni G, Nordberg A, Lubberink M. Tracer kinetic analysis of (S)- ^{18}F -THK5117 as a PET tracer for assessing tau pathology. *J Nucl Med.* 2016 Apr;57(4):574-81.

Review articles

Frisoni GB, Boccardi M, Barkhof F, Blennow K, Cappa S, **Chiotis K**, Démonet JF, Garibotto V, Giannakopoulos P, Gietl A, Hansson O, Herholz K, Jack CR Jr, Nobili F, Nordberg A, Snyder HM, Ten Kate M, Varrone A, Albanese E, Becker S, Bossuyt P, Carrillo MC, Cerami C, Dubois B, Gallo V, Giacobini E, Gold G, Hurst S, Lönneborg A, Lovblad KO, Mattsson N, Molinuevo JL, Monsch AU, Mosimann U, Padovani A, Picco A, Porteri C, Ratib O, Saint-Aubert L, Scerri C, Scheltens P, Schott JM, Sonni I, Teipel S, Vineis P, Visser PJ, Yasui Y, Winblad B. Strategic roadmap for an early diagnosis of Alzheimer's disease based on biomarkers. *Lancet Neurol.* 2017 Aug;16(8):661-676.

Chiotis K, Saint-Aubert L, Boccardi M, Gietl A, Picco A, Varrone A, Garibotto V, Herholz K, Nobili F, Nordberg A; Geneva Task Force for the Roadmap of Alzheimer's Biomarkers. Clinical validity of increased cortical uptake of amyloid ligands on PET as a biomarker for Alzheimer's disease in the context of a structured 5-phase development framework. *Neurobiol Aging.* 2017 Apr;52:214-227.

Saint-Aubert L, Lemoine L, **Chiotis K**, Leuzy A, Rodriguez-Vieitez E, Nordberg A. Tau PET imaging: present and future directions. *Mol Neurodegener.* 2017;12(1):19.

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LIST OF ABBREVIATIONS

A β	Amyloid- β
AD	Alzheimer's disease
ADNI	Alzheimer's disease neuroimaging initiative
ApoE4	Apolipoprotein E ϵ 4
APP	Amyloid precursor protein
BP _{ND}	Non-displaceable binding potential
CBD	Corticobasal degeneration
CSF	Cerebrospinal fluid
DiMI	Diagnostic molecular imaging
DVR	Distribution volume ratio
[¹⁸ F]FDG	2-[¹⁸ F]fluoro-2-deoxy-D-glucose
FSIQ	Full-scale intelligence quotient
MAPT	Microtubule-associated protein tau
MCI	Mild cognitive impairment
MMSE	Mini-mental state examination
MNI	Montreal Neurological Institute
MAO	Monoamine oxidase
MRI	Magnetic resonance imaging
NFT	Neurofibrillary tangle
PET	Positron emission tomography
PSP	Progressive supranuclear palsy
ROI	Region of interest
SCD	Subjective cognitive decline
SUV _R	Standardised uptake value ratio
TDP-43	TAR DNA-binding protein 43

1 INTRODUCTION

1.1 FROM NORMAL AGEING TO DEMENTIA

1.1.1 Ageing

Age-related progressive decline in intrinsic physiological functioning, associated with increased morbidity and mortality, is a common definition of ageing. ^{1,2} In the brain, normal ageing is linked with various structural and functional changes that are associated with a gradual decline in specific cognitive functions (e.g. processing speed, memory, etc.), which do not interfere with the activities of daily living. ³ However, the links between normal cognitive ageing and the age-related neurodegenerative diseases that lead to substantial cognitive deficits and functional disability remain elusive.

1.1.2 Dementia

Dementia can be described as the acquired loss of cognitive function, severe enough to interfere with daily life, caused by brain disease or injury. ⁴ According to the Diagnostic and Statistical Manual of Mental Disorders, 5th edition, the diagnosis of major neurocognitive disorder (previously dementia) diagnosis is mainly based on evidence of significant cognitive decline from a previous level of performance in one or more cognitive domains (complex attention, executive function, learning and memory, language, perceptual-motor, or social cognition), with these cognitive deficits interfering with independence in everyday activities. The diagnosis is made after the exclusion of other mental disorders that could explain the cognitive deficits (e.g. major depressive disorder, schizophrenia). ⁵

According to the Centers for Disease Control and Prevention USA, dementia is the sixth leading cause of death, behind heart disease, cancer, chronic lower respiratory diseases, accidents and stroke. More specifically, one in three seniors die with dementia, and 46 million people are estimated to live with dementia worldwide. ⁶ In Sweden it is estimated that more than 160,000 people suffer from dementia at the moment, ⁷ a prevalence comparable to that in other European countries. It is worth mentioning that, as age is the strongest known risk factor for dementia, the prevalence of dementia is expected to nearly double every 20 years, due to the global increase in population size and life expectancy, according to the World Alzheimer Report. ⁸ Dementia is not only associated with disability and mortality but also with dependence and societal costs, which place a great burden on families, communities and societies, especially since dementia is a terminal condition and the patients live for many years after the onset of symptoms. ⁹ It is noteworthy that the total worldwide cost of dementia in 2015 was US\$ 818 billion and is set to reach US\$ 2 trillion annually by 2030. ⁸ The annual cost of dementia in Sweden is calculated to exceed the SEK 60 billion in total, or SEK

398,000 per person with dementia per year.¹⁰ A growing body of evidence illustrates the dramatic increase in global prevalence and societal costs of the ‘dementia epidemic’¹¹ and highlights the need for prioritising dementia in the public health research agenda internationally.

1.1.2.1 *The spectrum of dementia*

The set of symptoms grouped under the general term dementia do not refer to a single clinico-pathological entity, but rather to several diseases with distinct characteristics, although a substantial clinical and pathological overlap between them has been observed. Alzheimer’s disease (AD) is the most common neurodegenerative disorder and cause of dementia, accounting for 50-70% of all dementia cases.¹² Other causes of dementia include frontotemporal lobar degeneration, vascular dementia, Lewy body disease, etc. (Figure 1). It should be noted that dementias with mixed underlying pathologies are a common finding; these show increased prevalence with increasing age.¹³ Finally, other diseases have been linked to dementia (e.g. Down’s syndrome, traumatic brain injury, Parkinson’s disease, Huntington’s disease, Creutzfeldt-Jakob disease) or dementia-like syndromes that may be reversed with the appropriate treatment (e.g. delirium, pseudodementia, infections, etc.).

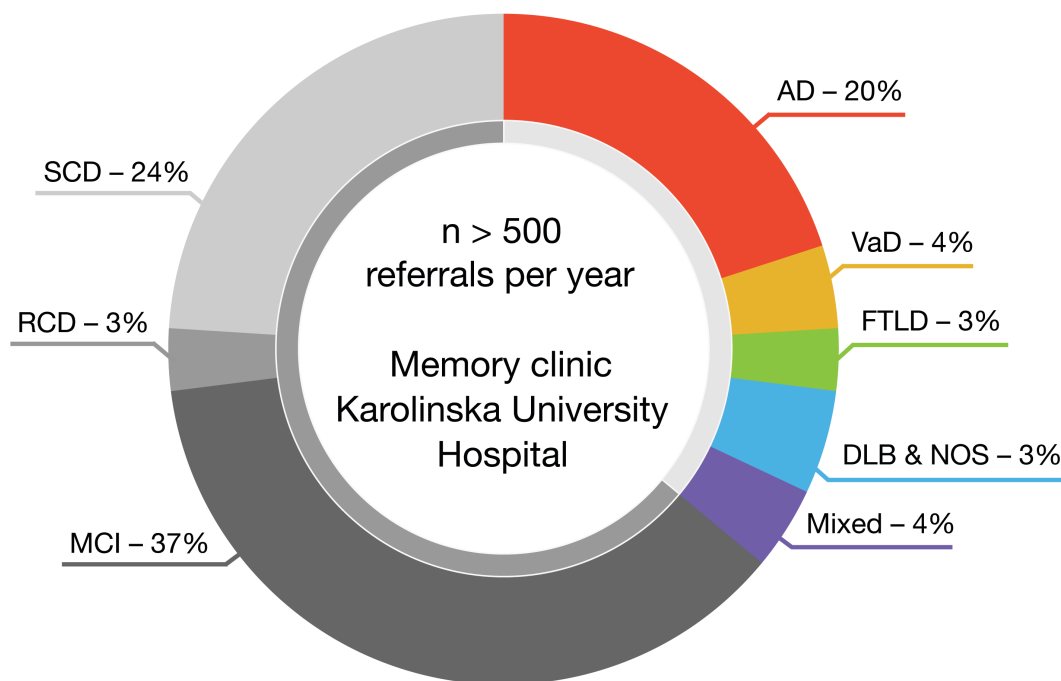


Figure 1. Pie chart illustrating the distribution (percentage, %) of diagnoses following memory assessment of more than 500 patients at the memory clinic, Karolinska University Hospital, Sweden, over one year (data from 2015). The coloured slices show the frequency of a diagnosis of dementia syndrome (34% in total). DLB = dementia with Lewy bodies; FTLD = frontotemporal lobar degeneration; Mixed = mixed dementia; NOS = dementia not otherwise specified; RCD = reversible cognitive disorder due to other medical conditions; VaD = vascular dementia.

1.1.3 Mild cognitive impairment

Mild cognitive impairment (MCI) is a clinical diagnosis with heterogeneous underlying causes that is thought to represent an intermediate stage between normal ageing and the diagnosis of dementia.¹⁴ The diagnosis is assigned in the presence of objective cognitive decline in one or more cognitive domains that is not expected for the age and education of the patient, and normal activities of daily living in the absence of a dementia disorder. Subsequent revisions of the diagnostic criteria have classified patients with MCI into four categories based on the impairment of memory and/or other cognitive domains;¹⁵ predominant impairment of memory has been more closely associated with later progression to AD.^{16,17} The diagnosis of MCI represents a risk factor for a subsequent dementia diagnosis,¹⁸ although not all patients will eventually develop dementia; a substantial number of patients will remain stable or even reverse to normal cognition over time.^{19,20}

1.1.4 Subjective cognitive decline

A substantial percentage of patients presenting with cognitive complaints are discharged with a clinical diagnosis of subjective cognitive decline (SCD) (Figure 1). The diagnosis is made in the presence of a self-perceived decline in cognitive performance, not related to an acute event, and normal performance on standardised cognitive tests, adjusted for individual age and educational attainment.^{21,22} Individuals with SCD represent an etiologically heterogeneous group with a subset of individuals developing objective cognitive deficits in the future. Although observations suggest that SCD is a risk factor for future development of MCI or dementia,²³⁻²⁶ the relationship over time between subjective and objective cognitive decline remains unclear and has attracted great interest from the scientific community.

1.2 ALZHEIMER'S DISEASE

In 1984, McKhann, et al.²⁷ in a working group established by the National Institute of Neurological and Communicative Disorders and Stroke and the Alzheimer Disease and Related Disorders Association (now Alzheimer's Association), defined AD as 'a brain disorder characterised by progressive dementia that occurs in middle or late life'. The pathological characteristics of the disease include the presence of neurodegeneration, neuritic plaques and neurofibrillary tangles (NFTs), as discussed below. Clinically, the disease usually manifests after the sixth decade of life, typically starting with impairment of short-term memory early in the disease course, before the development of more extensive cognitive deficits. However, the clinical presentation of the disease can be heterogeneous, with different clinical phenotypes described,²⁸⁻³⁰ and substantial overlap could exist in the clinical symptomatology of AD and other dementia syndromes.³¹

According to the most widely accepted diagnostic criteria,¹⁶ a diagnosis of AD can be made clinically in the presence of a progressive dementia disorder with two confidence levels

(namely, possible and probable). A probable diagnosis is made in the presence of dementia with deficits in at least two cognitive domains, progressive cognitive decline, no disturbance of consciousness, and onset of the disease after 40 years of age and after the exclusion of other systemic or brain diseases; a possible diagnosis is made with an atypical clinical presentation or in the presence of other significant diseases. Finally, a definite diagnosis of AD can only be assigned in the presence of histopathological evidence of the disease in autopsy or biopsy specimens.³² The level of uncertainty described in the clinical criteria for AD reflects the only moderate agreement between the clinical and neuropathological diagnoses,³³ as well as the absence, until very recently, of reliable laboratory or *in vivo* imaging markers of the underlying pathology.

While the cause of AD remains elusive, a number of risk factors have been identified. Specifically, increasing age, carriage of the apolipoprotein E ϵ 4 (ApoE4) allele, family history and low educational attainment are associated with increased prevalence of sporadic AD.³⁴⁻³⁶ A number of modifiable cardiovascular risk factors have been associated with increased risk of AD, including the presence of diabetes, obesity, smoking, hypertension, hypercholesterolaemia, and the lack of physical activity.³⁷

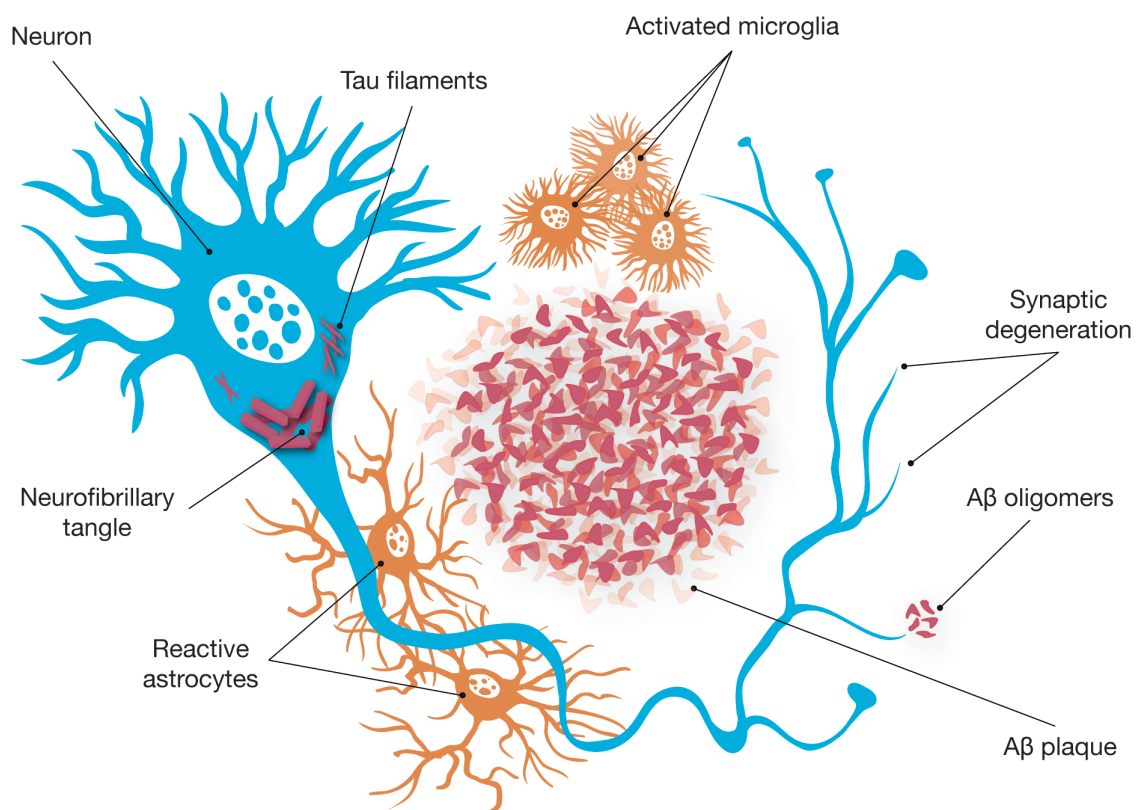


Figure 2. Illustration of the main pathological features of AD. Extracellular deposits of A β fibrils together with other proteins form the A β plaques, while intracellular deposits of tau filaments form the neurofibrillary tangles in AD. Inflammatory cells (i.e. reactive astrocytes and activated microglia) surround the A β plaques.

1.2.1 Neuropathology

Alois Alzheimer in 1906 was the first to identify and describe the neuropathological characteristics of a ‘peculiar severe disease process of the cerebral cortex’ later named after him, as Alzheimer’s disease. The characteristics of AD in the first patient to be described consisted of the presence of miliary foci of silver-staining deposits (later known as neuritic plaques), and bundles of fibrils (later known as NFTs), along with atrophy in the brain.³⁸

1.2.1.1 Amyloid- β plaques

Amyloid- β (A β) plaques are extracellular fibrillar deposits of insoluble A β protein (Figure 2).^{39,40} A β protein is formed by the cleavage, by β - and γ -secretases, of the parent molecule, the amyloid precursor protein (APP; gene located on chromosome 21), an integral membrane protein.^{41,42} A β is released extracellularly, and under normal conditions is mainly cleared into the cerebrospinal fluid (CSF) and later removed by the blood.⁴³ An imbalance between A β production and clearance in AD is thought to lead to the abnormal accumulation of the protein.⁴⁴ A β monomers aggregate into oligomers and these, based on the conformation they adopt, can be categorised into fibrillar-insoluble (β -sheet structure) or prefibrillar-soluble forms.⁴⁵ The insoluble forms are further aggregated into longer A β_{40} or A β_{42} β -sheet fibrils (Figure 3). Of note, A β_{42} is considered the most toxic species of A β . The A β fibrils together with other deposited proteins (e.g. ApoE, interleukins, complement, etc.) form the extracellular A β plaques.⁴⁶ Two types of plaque have been described, based on their morphology; diffuse and dense-cored plaques.⁴⁷ Neuritic plaques are a specific subtype of dense-cored plaques that consist of A β deposits surrounded by dystrophic neurites rich in deposits of abnormally hyperphosphorylated tau protein.⁴⁸

The evolution of the regional distribution of A β plaques during the course of AD has been described in detail; the neocortex is the first to be involved (Phase 1), followed by the hippocampus and entorhinal cortex (Phase 2), the basal ganglia (Phase 3), the brainstem (Phase 4) and finally, the cerebellum (Phase 5).^{49,50} The development of A β plaques is thought to start affecting the cortex in 4% of all neuropathology cases in the fourth decade, with A β pathology estimated to become prevalent in

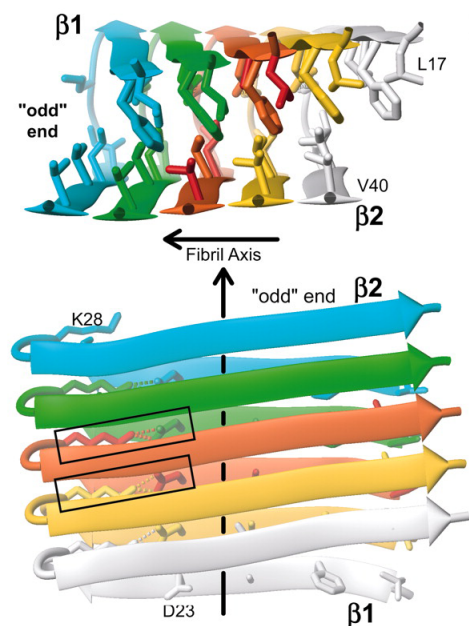


Figure 3. The 3D structure of an A β_{42} fibril obtained by using hydrogen-bonding constraints in quenched hydrogen/deuterium-exchange nuclear magnetic resonance. The fibril consists of two stacked, parallel β -sheets. Adapted with permission from Luhers, T. et al. 3D structure of Alzheimer's amyloid-beta(1-42) fibrils. *Proceedings of the National Academy of Sciences of the United States of America* **102**, 17342-17347, (2005). Copyright 2005 National Academy of Sciences.

more than 50% of all individuals in the eighth decade of life.⁵¹ Given the fact that a diagnosis of AD is typically made after the sixth decade and that the incidence rate of clinical AD, even in the eighth decade, does not exceed the 5%,⁵² it is apparent there is a long preclinical phase of A β accumulation and that a large number of individuals carry a substantial amount of A β pathology without ever developing the disease.

1.2.1.2 Tau pathology

The bundles of fibrils (NFT) that Alois Alzheimer described were in fact intraneuronal aggregates of the abnormally hyperphosphorylated microtubule-associated protein tau (MAPT) (Figure 2).⁵³ Tau protein, a cytoskeletal component that is abundant in the neuronal axons, plays an important role in regulating neuronal growth and axonal transport and stabilising the structure of the microtubules, a function that is regulated by the normal phosphorylation of tau.^{54,55} More specifically, the dephosphorylated tau binds to the microtubules and promotes their polymerisation, while its phosphorylation causes tau to dissociate from the microtubules. Tau is encoded in the MAPT gene in chromosome 17, and alternative mRNA splicing of the gene leads to six possible tau isoforms, three with three and three with four microtubule-binding domain repeats (i.e. 3R and 4R, respectively).⁵⁶ While in the foetus the predominant form of tau is the 3R form, which binds less stably to microtubules, in the healthy adult brain the 3R and 4R isoforms are equally expressed.⁵⁷ Although tau is most abundant in neurons, astrocytes and oligodendroglia also contain tau,

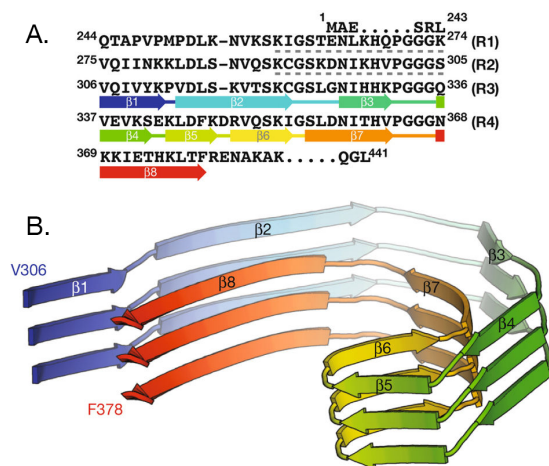


Figure 4. The 3D structure of the tau protofilament core obtained by cryo-electron microscopy. (A) Sequence alignment of the four microtubule-binding repeats (R1–R4) with the observed eight β -strand regions coloured from blue to red. (B) Rendered view of the secondary structure elements in three successive rungs. Adapted with permission from Macmillan Publishers Ltd: Nature, Fitzpatrick, A. W. P. *et al.* Cryo-EM structures of tau filaments from Alzheimer's disease. *Nature* **547**, 185-190, (2017). Copyright 2017.

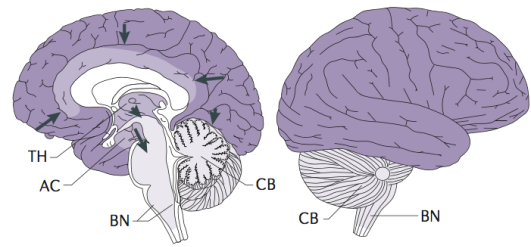
although this is essentially the 4R tau isoform.^{58,59} Both 3R and 4R tau undergo pathological hyperphosphorylation in AD, in contrast to other less common neurodegenerative diseases involving accumulation of tau protein (aka tauopathies), where there is predominant involvement of either 3R or 4R tau.⁶⁰ The hyperphosphorylation is followed by the aggregation of tau into β -sheet paired helical filaments (Figure 4), which form the insoluble NFTs intracellularly.⁵³ Although, under normal conditions, tau is located mainly in the axons of the neurons, the aggregation of tau leads to its redistribution to the soma and dendrites of the affected neurites.⁶¹ Three stages of aggregation of NFTs have been described, namely the pre-tangles (non-filamentous soluble aggregates), the intracellular mature tangles (condensed fibrillar deposits) and the extracellular ghost tangles (which arise after the death of the

neuron containing the mature tangles, named ‘tombstone’ lesions).^{62,63} Recent evidence suggests that there are differences in the tau isoform profile in the different stages of NFT deposits. A profile shift is observed from the predominantly 4R tau deposits in the non-fibrillar pre-tangles to predominantly 3R tau in the ghost tangles, while equal expression of isoforms is reported in the mature NFT.⁶⁴ Based on autopsy studies tau pathology, but not A β accumulation, has been closely associated with both neuronal loss and cognitive impairment in patients with AD, and it is thought to be a marker of progression of AD.⁶⁵⁻⁶⁸ However, although tau aggregation could lead, according to the current hypothesis, to cell death due to disruption of microtubule stability and axonal transport, the underlying mechanism is poorly understood.^{55,69-71} To add to this uncertainty, there is experimental evidence suggesting that neurons can tolerate a substantial amount of tau pathology for longer intervals than expected, raising the possibility that NFT formation could even act protectively against neuronal loss.⁷²⁻⁷⁴

The regional distribution of NFTs in AD evolves

in a predictable manner over time starting from the transentorhinal cortex and progressively affecting the hippocampus, the adjacent inferior temporal lobe, the cortical association areas and finally the primary cerebral cortices.^{49,75} It should be noted that the exact area of initial NFT deposition remains controversial, since it is thought that the tau pathology could be detected in the brain stem, and more specifically in the locus coeruleus, before it affects the transentorhinal cortex.⁷⁶ Most autopsy studies published to date have highlighted the importance of the localisation of the NFT deposits, especially in relation to the cognitive performance of the individual affected.⁷⁷ While NFT pathology in the medial temporal lobe is considered to be asymptomatic, in other words to be an inevitable process of ageing,⁵¹ spreading of the pathology to the adjacent neocortex has been associated with cognitive impairment, while severe dementia is thought to occur when the whole neocortex is affected.⁷⁸ The stereotypical propagation of tau pathology has led researchers to suggest that the pathology could spread in a prion-like manner. According to this hypothesis, the formation of misfolded tau aggregates in affected neurons could be transmitted to other neurons where the aggregates act as templates for the seeded aggregation of the native tau in the ‘healthy’ neuron. There is evidence of this from experimental studies in animal models and this represents a promising area for future research (for a detailed review, see⁷⁹⁻⁸¹).

A. A β plaques



B. NFT

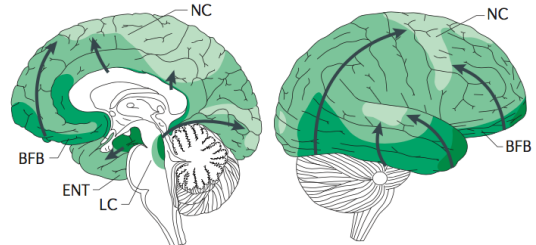


Figure 5. Illustration of the temporal spreading of (A) A β plaques and (B) NFTs in the AD brain. AC = allocortex; BFB = basal forebrain; BN = brainstem nuclei; CB = cerebellum; ENT = entorhinal cortex; LC = locus coeruleus; NC = neocortex; TH = thalamus. Adapted with permission from Macmillan Publishers Ltd: Nature reviews. Neuroscience, Brettschneider, J., Del Tredici, K., Lee, V. M. & Trojanowski, J. Q. Spreading of pathology in neurodegenerative diseases: a focus on human studies. *Nature reviews. Neuroscience* **16**, 109-120, (2015). Copyright 2015.

Although both A β plaques and NFTs follow stereotypical spatial spreading in the AD brain, the propagation profiles of the two pathologies are substantially different, as demonstrated in Figure 5. A long preclinical phase of NFT aggregation has been proposed, based on *post-mortem* studies; ^{82,83} data from these studies suggest that the formation of NFTs could even precede A β plaque deposition in the course of AD. ⁸⁴⁻⁸⁷

1.2.1.3 Neurodegeneration

The AD brain is characterised by macroscopic atrophy with decreased brain weight and enlargement of the ventricles. ⁸⁸ Microscopically, the neurodegeneration is expressed by neuronal loss and reduced synaptic density in both allo- and neo-cortical areas, which correlates closely with the cognitive function of the patient (Figure 2). ⁸⁹⁻⁹² More specifically, changes in synaptic integrity are observed, with degeneration of the axons and subsequent neuronal death. ^{93,94}

1.2.1.4 Neuroinflammation

Neuroinflammation in AD is not limited to the presence of interleukins and component proteins in association with A β plaques. ⁹⁵ Autopsy studies have revealed the existence of both activated microglia and reactive astrocytes proximal to A β plaques (Figure 2). ⁹⁶⁻⁹⁸ Microglial cells are inflammatory cells that can be primed (multiplied and activated) in response to their microenvironment. Activated microglia are characterised by pro-inflammatory and anti-inflammatory states, and are partly involved in the phagocytic clearance of A β . ⁹⁹ Reactive astrocytes have diverse phenotypes, ¹⁰⁰ and although they have been associated with the clearance of A β ¹⁰¹ their role seems more complex. Specifically, it has been suggested that reactive astrocytes could play an additional role in both A β accumulation and the induction of oxidative stress. ¹⁰²⁻¹⁰⁴

1.2.1.5 Neuropathological criteria

Despite intense efforts to develop biomarkers that will detect *in vivo* changes in the AD brain, *post-mortem* neuropathological evaluation remains the gold standard in the diagnosis of AD. The recently described neuropathological criteria ^{32,105} for an AD diagnosis are based on a combination of the assessments of the phases of A β plaques development, ⁵⁰ the stages of NFT spreading ^{49,106} and a semi-quantitative assessment of the neuritic plaque load. ¹⁰⁷

1.2.2 Amyloid cascade hypothesis

The amyloid cascade hypothesis, formulated in 1992 by Hardy and Higgins¹⁰⁸, is still the most widely accepted conceptualisation of the pathogenesis of AD. The factors that led to formulation of the hypothesis include the identification of mutations in the APP gene (chromosome 21) as deterministic for the development of autosomal dominant AD,^{109,110} and the very high prevalence of the disease in patients with Down's syndrome (trisomy 21).^{40,111,112} According to this hypothesis, A β plays a central role in the neuropathology of the disease, with its accumulation leading to the abnormal hyperphosphorylation of tau protein and neurodegeneration. However, through the years, a number of weaknesses have tested the validity of this hypothesis.¹¹³ For example, A β deposition is common in cognitively normal elderly;¹¹⁴ then the animal models with overexpression of the APP gene do not develop substantial neurodegeneration or the AD phenotype of cognitive impairment;^{115,116} A β accumulation does not show a close relationship with cognitive impairment, especially at the symptomatic stages of the disease;⁶⁵ and anti-A β drugs have, so far, failed to change the course of the disease, at least in its later stages.¹¹⁷⁻¹¹⁹

Refinement of the amyloid hypothesis^{120,121} and alternative models of AD pathogenesis has been proposed in order to account for the weaknesses of the hypothesis formulated by Hardy and Higgins¹⁰⁸. A β -soluble oligomers are thought, now, as the most neurotoxic form of A β aggregates that could drive tau pathology, although our knowledge about their role remains fragmentary.¹²²⁻¹²⁶ According to this hypothesis, the fibrillar A β plaques may not be harmful but will instead act as 'inert sinks' for the accumulation of A β oligomers.

Alternative models, where tau pathology or neuroinflammation are of central interest, have also been proposed,^{84,121,127-129} although these have received less attention to date.

1.2.3 Cognitive performance

The term neuropsychological assessment is used to describe the administration of a number of tests for evaluation of the cognitive function and functional status of an individual. The assessment typically evaluates the performance in different cognitive domains (i.e. memory, perception, attention, language, visuospatial ability and executive function) and it is being used extensively in the clinical examination of patients with cognitive symptoms. On an individual level neuropsychological test results can be compared to age/education matched normative data (or z-scores from a population mean) and similarly results can be compared statistically on a group level e.g. age/education matched cognitively normal individuals compared to patient groups. Both individual and group level comparisons allow neuropsychologists to determine whether cognitive impairment is present in that person/group. The selective impairment of episodic memory is thought to be an early sign of AD, and has been associated with neurodegeneration in the medial temporal lobe, particularly the hippocampus.¹³⁰ Furthermore, the progression of the pathology in the neocortex is associated with additional impairment in other cognitive domains.¹³¹ Overall, although

neuropsychological testing is very sensitive to the detection of cognitive deficits in relation to the cognitive background of the individual,¹³² it is not highly accurate alone in the differential diagnosis of the underlying pathology.¹³³

1.3 CORTICOBASAL DEGENERATION AND PROGRESSIVE SUPRANUCLEAR PALSY

Corticobasal degeneration (CBD) and progressive supranuclear palsy (PSP) are two neuropathological entities characterised by the aggregation of abnormally hyperphosphorylated tau protein; tau aggregates are localised in neurons (i.e. neurofibrillary

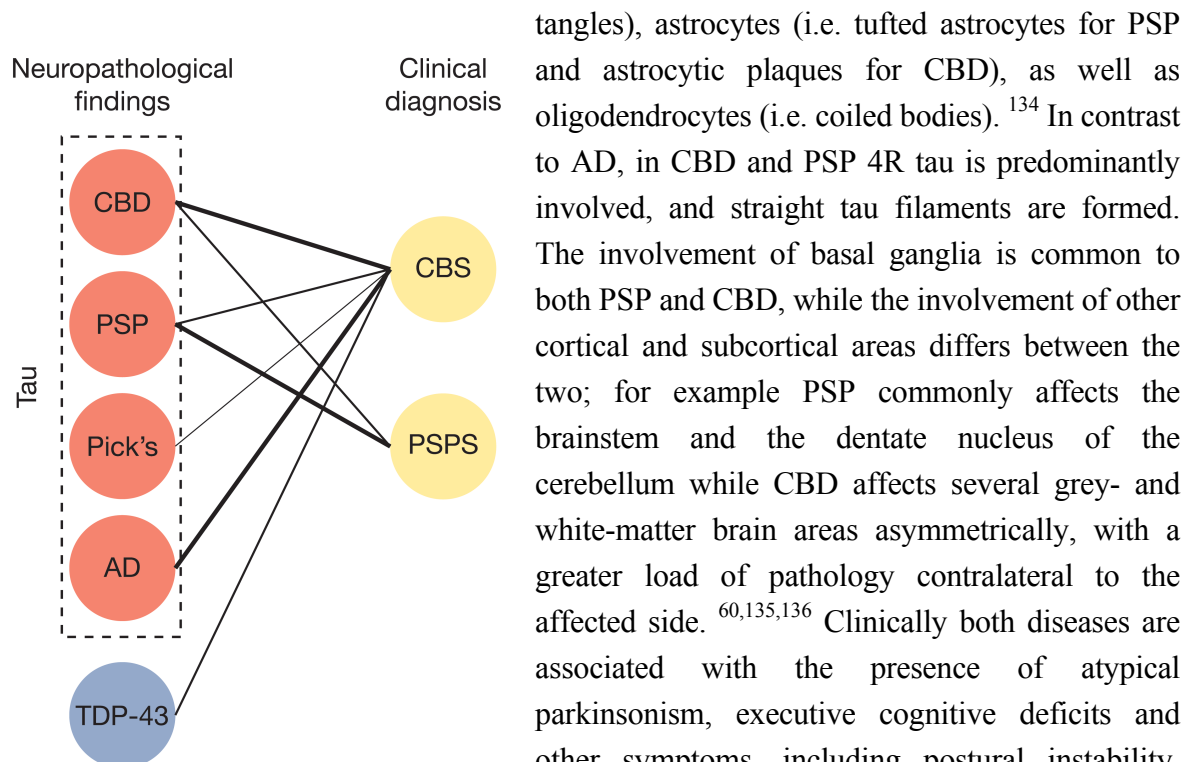


Figure 6. Atypical parkinsonian syndromes (right panel) and associated neuropathological findings (left panel). The weight of the strings in the diagram illustrates the approximate strength of the clinicopathological correlations. CBS = corticobasal syndrome; Pick's = Pick's disease; PSPS = progressive supranuclear palsy syndrome. Figure inspired by Miller, B. L. & Boeve, B. F. *The behavioral neurology of dementia*. 2nd edition, Cambridge University Press, (2016) and Rohrer, J. D. & Rosen, H. J. *Neuroimaging in frontotemporal dementia*. *International review of psychiatry* **25**, 221-229, (2013).

tangles), astrocytes (i.e. tufted astrocytes for PSP and astrocytic plaques for CBD), as well as oligodendrocytes (i.e. coiled bodies).¹³⁴ In contrast to AD, in CBD and PSP 4R tau is predominantly involved, and straight tau filaments are formed. The involvement of basal ganglia is common to both PSP and CBD, while the involvement of other cortical and subcortical areas differs between the two; for example PSP commonly affects the brainstem and the dentate nucleus of the cerebellum while CBD affects several grey- and white-matter brain areas asymmetrically, with a greater load of pathology contralateral to the affected side.^{60,135,136} Clinically both diseases are associated with the presence of atypical parkinsonism, executive cognitive deficits and other symptoms, including postural instability, ophthalmoparesis or progressive apraxia, depending on the regional distribution of the underlying pathology.¹³⁷⁻¹³⁹ The clinical syndromes associated with PSP and CBD (PSP and corticobasal syndromes, respectively), however, could be difficult to distinguish, since the diseases show a substantial clinical and neuropathological overlap (Figure 6).¹⁴⁰⁻¹⁴⁴ Moreover, these syndromes have also been associated with neuropathological evidence of AD or with the presence of tau-negative inclusions, which further complicates the reliable clinical diagnosis in those patients.^{145,146}

1.4 BIOMARKERS

‘Biomarker: A characteristic that is objectively measured and evaluated as an indicator of normal biological processes, pathogenic processes, or pharmacologic responses to a therapeutic intervention’ as defined by the Biomarkers Definitions Working Group.¹⁴⁷

A number of biomarkers have recently been employed to help in the differentiation of neurodegenerative diseases and causes of dementia, aiming for early detection and staging of the pathology, and are also being used to monitor the therapeutic efficacy of disease-modifying drugs.¹⁴⁸ Investigation into the clinical validity of two of these, molecular imaging and CSF markers, has progressed furthest relative to other biomarkers.

1.5 MOLECULAR IMAGING

Advanced neuroimaging techniques have allowed imaging of structural and functional biological abnormalities *in vivo*. Computed tomography, magnetic resonance imaging (MRI) and positron emission tomography (PET) are only some of the developed imaging technologies; each modality presents with different advantages and limitations. While computed tomography and structural MRI were developed for imaging the structure of systems clinically, PET allows the imaging and quantification of biochemical processes *in vivo* by incorporating positron-emitting isotopes into molecular radiotracers.¹⁴⁹

1.6 MAGNETIC RESONANCE IMAGING

Structural imaging of the brain with MRI offers highly sensitive detection *in vivo* of brain abnormalities such as atrophy, trauma, tumours, vascular changes (i.e. stroke, bleeding, etc.), mass lesions and other intracranial findings. MRI does not use ionising radiation but instead uses combination of magnetic fields, radio waves, and field gradients to image the anatomy of the brain with a wide range of contrasts. Several studies in the field of neurodegeneration have highlighted differences in terms of atrophy between cognitively normal individuals and patients with cognitive impairment, and have also shown that it is possible to discriminate between the different underlying causes of neurodegeneration and dementia, based on specific atrophy patterns.^{150,151} More specifically, in AD atrophy changes have been typically observed in temporo-parietal areas, including the medial temporal lobe,¹⁵² although atrophy variants have also been observed in patients with AD.¹⁵³ The extent of atrophy has been associated with *post-mortem* evidence of neuronal loss, with the underlying NFT pathology as well as with cognitive decline and is considered a very good marker of disease progression.¹⁵⁴⁻¹⁵⁷ Visual scales of medial temporal atrophy¹⁵⁸ have been part of the diagnostic assessment in specialised memory units with good accuracy in discriminating between patients with dementia from cognitively normal volunteers, although it has proven less useful in differentiating between different causes of dementia. The use of automatic

procedures for measuring patterns of atrophy might lead to wider use of MRI imaging in the differential diagnosis of the different causes of cognitive impairment.¹⁵⁹

Several MRI sequences have been developed in recent years to allow the imaging of different physiological processes, which widens the application of MRI in the field of neurodegeneration. These include imaging of cerebral blood flow with arterial spin labelling, imaging cerebral connectivity using diffusion weighted imaging sequences, measuring cerebral activation with functional MRI, and detecting levels of metabolites using spectroscopy sequences.¹⁶⁰⁻¹⁶³ However, clinical validation of these techniques is still pending.

1.7 POSITRON EMISSION TOMOGRAPHY

The introduction of PET imaging allowed *in vivo* detection of the load and regional distribution of different molecular targets, based on the binding of specially designed tracers. The first human PET scanner was documented in 1976 at Washington University, St. Louis, USA, by Phelps, et al.¹⁶⁴ PET is based on the detection of a pair of 511 keV annihilation gamma-rays, which are produced after the β^+ decay of a positron-emitting short-lived radioactive isotope. Radioactive isotopes are atoms with unstable nuclei that release energy when they undergo decay, in order to be transformed in a more stable state. For the purposes of PET, isotopes that will undergo positron-emitting decay shortly after production (i.e. that

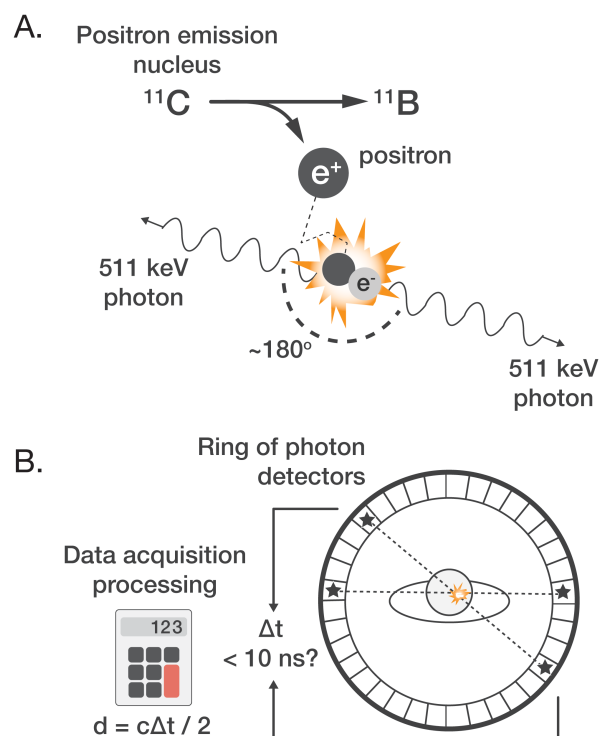


Figure 7. Illustration of the basic principles behind PET imaging. Δt = time between the arrival of each of the anti-parallel pair of photons; c = speed of light; d = distance from the detected annihilation to the midpoint of the scanner on the line connecting the coincidence events.

have a short half-life; e.g. ^{11}C , ^{18}F , ^{13}N and ^{15}O) are artificially produced in a particle accelerator called a cyclotron. These isotopes are incorporated into molecules (i.e. the molecules are labelled as tracers), which are known to target different biochemical processes, to form the radiotracer that will be injected into the patient. Following the injection, the radiotracer is distributed into specific areas in the body, based on its pharmacological characteristics, where it binds to its molecular target. When the isotope decays, the atom transforms one of its protons into a neutron and emits a positron. The positron travels a short distance before it ‘meets’ its anti-particle, the electron. The contact of the two will lead to their annihilation or, in other words, the transformation of their mass into energy, as detected by the production of an anti-

parallel (180°) pair of photons (gamma-rays; 511 keV each) (Figure 7A). The anti-parallel pair of photons is expected to reach detectors at each side of the ring of the PET scanner roughly at the same time ($\Delta t < 10$ ns). The scanner is able to record these coincidence events as deriving from the same annihilation. With the use of more advanced coincidence processing, the location of the annihilation can be determined on the line connecting the two activated photon detectors ($d = c \Delta t / 2$) (Figure 7B). The events recorded are later reconstructed as an image using computation algorithms. Detection of the pair of photons deriving from the same annihilation is the reason for the higher sensitivity of PET over other imaging modalities, even with the injection of very low concentrations of radiotracer. However, because of detector physics, PET is characterised by low resolution relatively to computed tomography or MRI, and therefore does not provide useful structural information.

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An ideal radiotracer should be able to penetrate the blood–brain barrier adequately without being a P-glycoprotein substrate, would have high affinity (binding affinity usually in nM range) and selectivity for the target with a low off-target signal, would have favourable pharmacokinetics for PET imaging (rapid brain uptake and wash-out), would lack radioactive metabolites able to cross the blood–brain barrier and, finally, would be safe for administration in low doses.¹⁶⁶ Different isotopes can be used for radiolabelling the tracers, each one with different advantages and disadvantages. Isotopes with a very short half-life (e.g. [¹¹C] with a 20 min half-life) have been very useful in the research setting, allowing multi-tracer PET imaging *in vivo* on the same day; they, however, require an on-site production. In contrast, isotopes with a longer half-life (e.g. [¹⁸F] with a 109 min half-life) can be produced in a cyclotron centrally and the radiolabelled tracers can be delivered to geographically dispersed sites, thus allowing the clinical application of the radiotracer even in centres without access to highly-specialised facilities and personnel. More than 40 radiolabelled tracers targeting specific biological processes have been developed through the years for the study of brain diseases.¹⁶⁷

1.7.1 Glucose consumption

2-[¹⁸F]fluoro-2-deoxy-D-glucose ([¹⁸F]FDG), a radiolabelled glucose analogue, is used as a PET tracer to measure metabolic glucose consumption within a targeted tissue. FDG is transported inside the cell, mediated by glucose transport proteins and is phosphorylated by hexokinase. However, unlike normal glucose, FDG cannot enter the glycolytic pathway and is trapped inside the cell, allowing the rate of trapping, and thus metabolic rates of glucose consumption to be approximated with dynamic PET imaging. Its use in neuroimaging, and dementia research, has been longstanding. A reduced [¹⁸F]FDG signal is associated with neurodegenerative changes including neuronal dysfunction, changes in synaptic activity and neuronal death.¹⁶⁸⁻¹⁷⁵ Recent evidence, however, is challenging the idea that the [¹⁸F]FDG signal reflects neuronal activity exclusively, since activated astrocytes may also contribute to the observed signal.¹⁷⁶ However, the contribution of each cell type remains elusive.

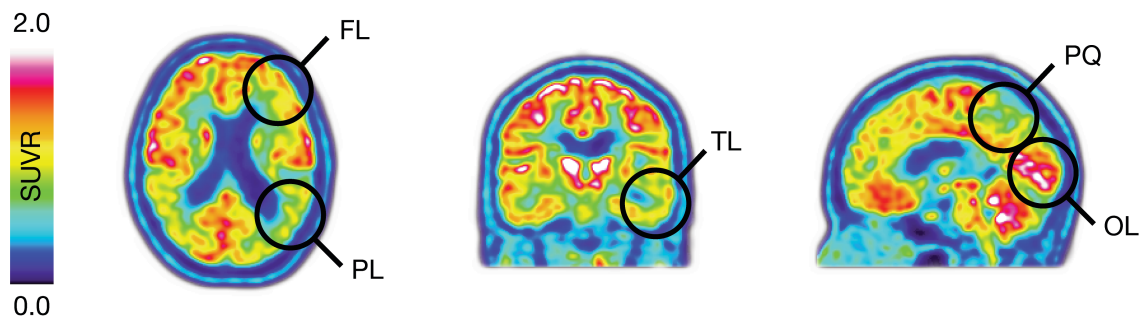


Figure 8. [^{18}F]FDG PET scan in a patient with a clinical diagnosis of probable AD, illustrating the areas typically affected in terms of glucose metabolism. The temporal (TL) and parietal (PL) lobes, including the precuneus (PQ), are primarily affected, and the frontal lobe (FL) is also (secondarily) affected. The metabolism of the occipital lobe (OL) remains relatively spared. The pons was used as the reference region for the quantification of [^{18}F]FDG uptake.

The uptake of [^{18}F]FDG is lower in patients with AD than in cognitively normal individuals, especially in the temporo-parietal association cortices, the precuneus and the posterior cingulate gyrus, also called the FDG signature regions for AD (Figure 8).^{177,178} [^{18}F]FDG uptake declines over time in patients with AD, in these cortical regions;¹⁷⁹ the change in uptake is closely correlated to cognitive decline in the patients.¹⁸⁰ Moreover, the exact spatial patterns of low uptake of [^{18}F]FDG tend to reflect the different clinicopathological variants of AD,¹⁸¹⁻¹⁸³ as well as to differentiate with high specificity between AD and other causes of dementia, including the different types of frontotemporal lobar degeneration or Lewy body disease.¹⁸⁴ Changes in uptake of [^{18}F]FDG have been observed even earlier than the onset of dementia, in patients with MCI,¹⁸⁵ although the pattern of changes appears heterogeneous, probably because of the different causes of MCI. At the MCI stage, [^{18}F]FDG has moderate-to-high sensitivity and specificity for discriminating between patients who could later develop clinical AD and those who could develop other types of dementia.^{150,186} The clinical validity of [^{18}F]FDG in the differential diagnosis of patients with cognitive complaints has been well established,¹⁸⁷ with [^{18}F]FDG PET currently being used in specialised memory units, typically as a second-line test where there is diagnostic uncertainty.

1.7.2 Fibrillar amyloid- β deposition

The identification of a fibrillar A β -specific tracer with favourable pharmacokinetics ([^{11}C]Pittsburgh compound B, [^{11}C]PIB) led to the first *in vivo* study in human published in 2004 (Figure 9A).¹⁸⁸ The PIB radiotracer was based on the structure of the fluorescent dye thioflavin T, which is widely used to detect beta-sheet structures, including A β fibrils and NFTs, in autopsied brain tissue or *in vitro* cultures. [^{11}C]PIB has high affinity for A β fibrils¹⁸⁹ and, injected *in vivo*, was adequately taken up and quickly washed out from the brains of the first study participants.¹⁸⁸ Patients with clinically probable AD have high binding of the tracer across the whole neocortex, with the medial temporal cortex relatively spared, in comparison with cognitively normal individuals (Figure 9B). Autopsy studies performed in patients who had undergone [^{11}C]PIB PET imaging *ante-mortem* have illustrated the selective

binding of [^{11}C]PIB in insoluble fibrillar A β deposits (predominantly dense-cored over diffuse plaques), including vascular A β pathology (i.e. cerebral amyloid angiopathy), and the strong correlation between *in vivo* [^{11}C]PIB binding and region-matched histopathological measures of A β pathology. Interestingly, in the cerebellum, a region commonly used as a reference for quantifying [^{11}C]PIB binding, diffuse A β plaques were not labelled with PIB. Moreover, PIB did not show evidence of binding to soluble forms of A β or to the NFTs. 179,190-192

The short half-life of [^{11}C] (~20 min), however, precludes its use in centres without on-site radiochemistry facilities, as previously discussed. This led to the development of [^{18}F] A β PET tracers with longer half-lives (~110 min), which enabled them to be produced centrally and be transferred to geographically dispersed sites, thus enabling their widespread use for research and in the clinic. Derivatives of PIB were used for the [^{18}F] A β PET tracers as can be seen by their chemical structures (Figure 9A). All the [^{18}F] tracers were highly comparable

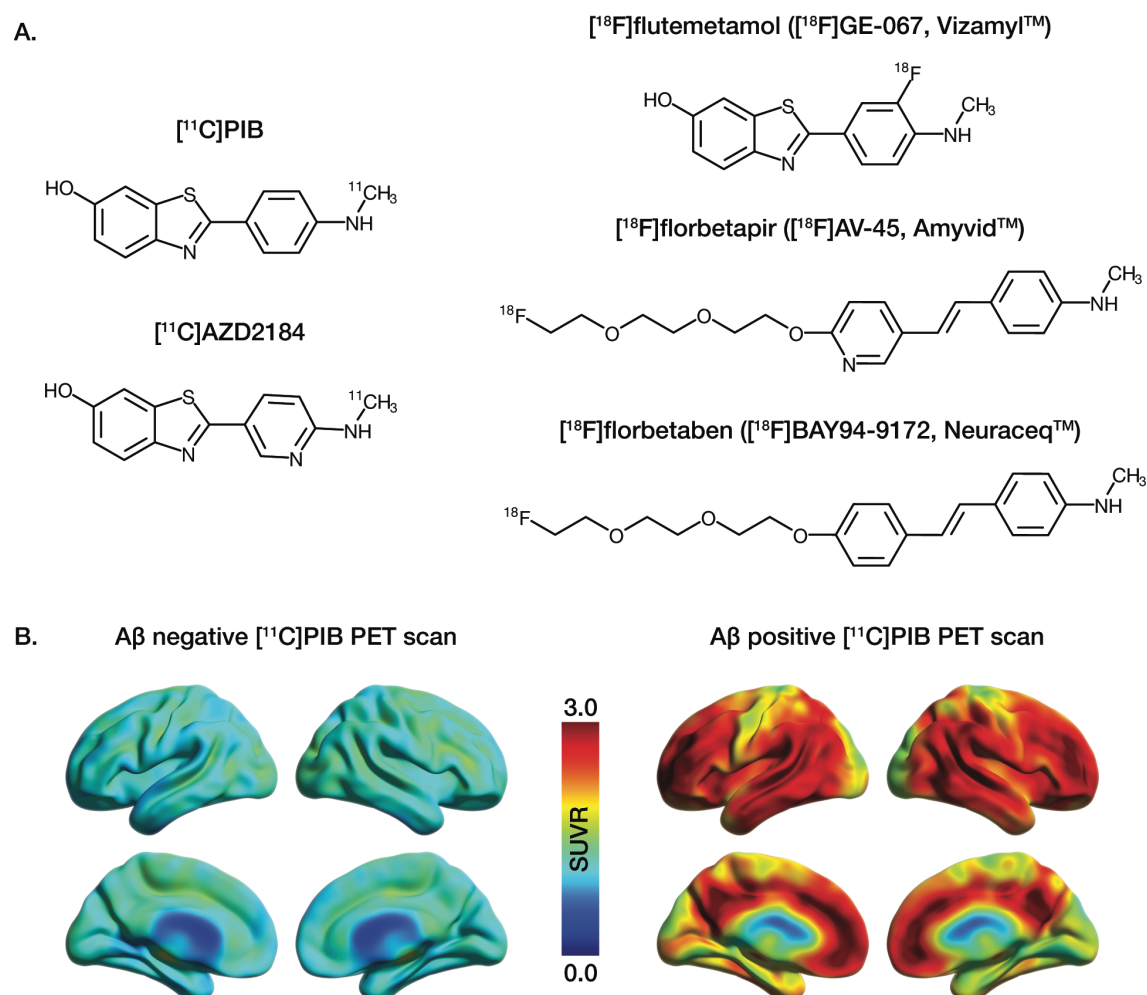


Figure 9. (A) Illustration of the chemical structures of A β -specific PET tracers. PIB and AZD2184 were labelled with [^{11}C] while flutemetamol, florbetapir and florbetaben were labelled with [^{18}F]. (B) Cortical projection of A β -positive and A β -negative PET scans. The scans were performed with [^{11}C]PIB in a cognitively normal individual (A β -negative; left panel) and a patient with a clinical diagnosis of probable AD (A β -positive; right panel). Cerebellar grey-matter was used as the reference region for quantifying [^{11}C]PIB binding.

with [^{11}C]PIB when examined in a head-to-head design, although they showed more extensive off-target binding.¹⁹³⁻¹⁹⁵ However, the comparability of [^{11}C]PIB and the [^{18}F] A β tracers when investigated in separate patient cohorts remained largely unexplored.

Available *in vivo* evidence with the different tracers shows that in cognitively normal individuals the prevalence of A β -positivity (A β PET binding above the cut-off for positivity) increases in an age-related manner,¹¹⁴ in agreement with previously published neuropathological studies,⁵¹ with >30% of individuals over the age of 80 exhibiting pathological levels of fibrillar A β (measured by A β PET).¹⁹⁶ The presence of the ApoE4 allele is associated with up to three times higher prevalence of A β -positivity in cognitively normal individuals.¹⁹⁶ The build-up of A β deposition, as imaged with PET, is a slow process that is thought to start at the preclinical, presymptomatic stage of AD; it can take more than a decade before the tracer binding exceeds the threshold of A β pathology. The models based on longitudinal PET imaging also suggest that the pathology continues to build up for at least another decade before it reaches a plateau in patients with AD dementia.^{179,197,198} Interestingly, patients with A β -negative MCI will not develop clinically probable AD – with a reported sensitivity of 96% – while patients with an A β -positive scan will be at high risk of the disease (specificity of 72%).¹⁹⁹⁻²⁰¹ However, many patients with A β -positive MCI will not develop probable AD based on different longitudinal studies, which probably reflects the relatively short follow-up intervals as well as confirming the neuropathological evidence suggesting that a substantial number of elderly possess AD pathology but do not clinically manifest AD during their life span.⁵¹

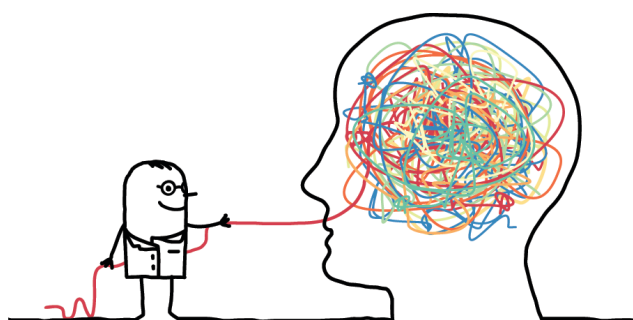
The introduction of [^{18}F] A β PET tracers allowed the validity of A β PET to be evaluated easily before its clinical incorporation. Furthermore, large validation studies with the different tracers have indicated that *in vivo* A β PET imaging is able to accurately show A β pathology that was later confirmed *post-mortem* – with a sensitivity and specificity that reached or exceeded 90% – further supporting the utility of PET imaging as a biomarker of A β deposition in the differential diagnosis of syndromes associated with cognitive impairment.²⁰²⁻²⁰⁶ Following the evidence from the validation studies, the US Food and Drug Agency and the European Medicines Agency recently approved three A β tracers ([^{18}F]florbetapir, [^{18}F]flutemetamol, [^{18}F]florbetaben) for excluding the presence of A β pathology in the clinical investigation of cognitive impairment. Since then, appropriate criteria for the clinical use of A β PET have been published,²⁰⁷ although the impact of other patient characteristics (e.g. age or ApoE4 carrier status) on the utility of this biomarker remains unclear. On-going large multi-centre studies are investigating the clinical validity of A β PET imaging in greater detail in Europe (Amyloid imaging to prevent Alzheimer's disease; AMYPAD) and the USA (Imaging Dementia – Evidence for Amyloid Scanning; IDEAS). Both these studies, and others, aim to evaluate the performance of A β PET in the management of patients with cognitive impairment and the cost-effectiveness of this imaging modality in a clinical setting.

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1.7.3 Tau pathology

The wide spectrum of degenerative tauopathies ²⁰⁸ and the close relationship between tau pathology, neurodegeneration and cognitive measures in AD, as reported by autopsy studies, ^{65,66} raised interest in the development of PET radiotracers that would allow *in vivo* imaging of tau. The addition of tau PET to the imaging arsenal would allow more light to be shed on the pathological events that lead to neurodegeneration, the differentiation of tauopathies, and the development of new disease-modifying therapies. Everything started with the development of [¹⁸F]FDDNP in 1999, a tracer that was originally designed to target A β pathology but that showed additional affinity for tau deposits. ²⁰⁹⁻²¹¹ However, the development of tau-specific PET tracers had been particularly challenging (Figure 10) ^{208,212} and it would take 10 more years before promising new tracers started to emerge. Tau is a very heterogeneous target since it exists in multiple isoforms, as discussed above, undergoes different post-translational modifications (i.e. phosphorylation, ubiquitination, truncation, etc.), ²¹³ and forms different types of filaments and deposits depending on the underlying tauopathies (Table 1). ^{134,208,214,215} The localisation of tau deposits also varies, as deposits are found in neurons and glial cells, in grey and white-matter, and in areas commonly used as reference regions in PET (i.e. brainstem and cerebellum). Furthermore, tau deposits are characterised by complex dynamic changes over time with distinct maturation stages. To add to the complexity of imaging tau pathology, the deposits are predominantly intracellular, in contrast to A β pathology, and therefore the tracer will need to pass both the blood-brain barrier and the cell membrane to reach the target. Furthermore, the common co-localisation of tau and A β deposits (i.e. neuritic plaques), with relative abundance of A β deposits in AD, could further complicate evaluation of the specificity of a potential tau tracer. Finally, since ‘normal’ tau is practically invisible even with immunohistochemistry techniques, ²¹⁶ the detection of ‘abnormal’ insoluble tau could be based on the adopted β -sheet conformations. However, caution is advised if this principle is applied to the design of a PET tracer, since the β -sheet formation is not specific to ‘abnormal’ tau but is the characteristic structure that is adopted by different misfolded proteins (‘amyloids’), associated with neurodegeneration (e.g. TAR DNA-binding protein 43 (TDP-43), α -synuclein or A β), and this could limit the

Disentangling the challenges of tau PET imaging



- Intracellular localisation of tau
- Multiple tau isoforms
- Post-translational modifications of tau
- Heterogeneous filament formation
- Deposits of tau in different cell types
- Different maturation stages of deposits
- Deposits in grey- and white-matter
- Tau and A β deposits coexist in AD
- Other misfolded proteins form similar β -sheets

Figure 10. Illustration of the challenges related to the development of tau-specific PET tracers.

specificity of the tau tracer.

Table 1. Common tauopathies and related biochemical and neuropathological characteristics of the underlying tau pathology.

Tauopathy	Isoforms	Filaments	Histopathological findings		Location
			Neurons	Glial cells	
AD	3R \approx 4R ^a	Paired helical >> Straight	NFTs Neuritic plaques Neuropil threads	–	Detailed staging by Braak and Braak ⁴⁹ , Delacourte, et al. ⁷⁵
CBD	4R > 3R	Straight >> Twisted	NFTs Neuropil threads Ballooned neurons	Astrocytic plaques Coiled bodies	Grey- and white-matter areas, striatum
PSP	4R > 3R	Straight	NFTs Neuropil threads	Tufted astrocytes Coiled bodies	Subthalamic nuclei, striatum, dentate nucleus, cortex ^b
Pick's disease	3R > 4R	Straight >> Twisted	Pick bodies Pick cells	–	Hippocampus, striatum, cortex

^a shift to 3R predominance in the extracellular 'ghost' tangles; ^b variable involvement of the cortex

Several families of tracers have been developed during the past seven years. The most widely used tracers are [¹⁸F]THK5317 and [¹⁸F]THK5351, which were developed at Tohoku University, Japan, [¹⁸F]AV-1451 (aka T807 or flortaucipir), which was developed by Siemens Medical Solution, USA, and sold to Avid Radiopharmaceuticals, USA (Eli Lilly & Co, USA), and [¹¹C]PBB3 which was developed by the National Institute of Radiological Sciences in Chiba, Japan (Figure 11A). The tracers showed *in vitro* high binding affinity to and specificity for tau deposits. Moreover, the binding patterns of the tracers in adjacent sections of AD brain tissue resembled the pattern of immunohistochemistry with tau-specific antibodies (e.g. AT8, PHF-1), further supporting the selectivity of the tracers for tau deposits. ²¹⁷⁻²²² There is so far scant evidence for specific targets of the different tracers on tau deposits, ²²³ and it would not come as a surprise if they bound to different molecular targets on tau pathology, given the heterogeneity of tau. Indeed, recent *in vitro* evidence has indicated that the different tracers may bind to different sites in the AD brain and are likely to image different aspects of 'abnormal' tau deposition in AD or other tauopathies. ^{224,225}

When the tracers were injected *in vivo*, they showed adequate brain uptake and rapid washout, although a radiolabelled metabolite of [¹¹C]PBB3 that was able to cross the blood-

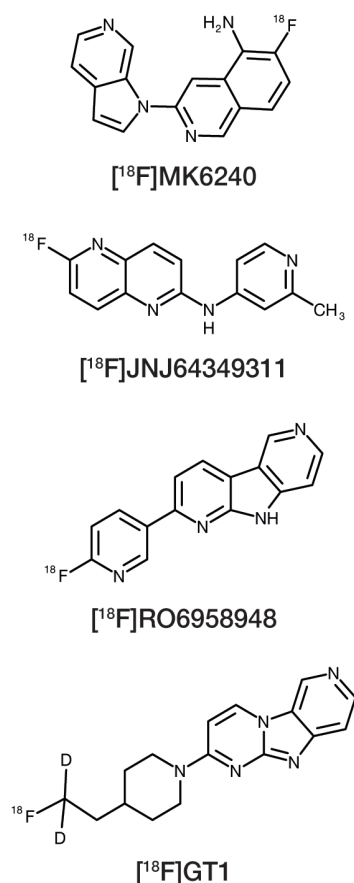


Figure 12. Chemical structures of newly developed tau-specific tracers that are considered to belong to the second generation of tracers with improved characteristics.

over time with other biomarkers of the disease, with the exception of the study included in this thesis (paper IV).

In patients with atypical parkinsonism and a clinical diagnosis associated with the presence of CBD or PSP pathologies, the tau tracers showed binding in brain areas expected from *post-mortem* studies.^{220,247-252} Moreover, there was agreement between areas with high tracer binding and tau pathology in patients who underwent autopsy evaluation, further illustrating that these tracers could prove useful in non-AD tauopathies.²⁵³⁻²⁵⁵ However, the fact that the tracers bind off-target to areas relevant for those tauopathies questions their usefulness in discrimination. Indeed, a recent study showed that there were no differences between patients with clinical PSP and cognitively normal participants.²⁵⁶ Concerns about off-target binding of the tracers have been raised not only with regard to imaging non-AD tauopathies but also with regard to the general validity of the tracers. Several potential sources of off-target binding have been suggested,^{236,257-261} although a thorough assessment, including direct comparisons between tracers, is pending.

Newly developed tau-specific tracers are thought to have improved binding properties with lower off-target signal, although no *in vivo* data have been published so far (Figure 12).

1.8 CEREBROSPINAL FLUID MARKERS

The identification and quantification of $\text{A}\beta$ in the CSF²⁶² led to the development of specific assays to measure the $\text{A}\beta_{42}$ isoform. The low levels of $\text{A}\beta_{42}$ in the CSF of AD patients are thought to reflect the deposition of $\text{A}\beta_{42}$ into plaques in the brains of these patients, and therefore its reduced clearance to the CSF.^{263,264} Indeed, an inverse relationship between the neuropathological $\text{A}\beta$ plaque load and CSF $\text{A}\beta_{42}$ measurements has been observed.^{265,266} However, although part of the scientific community treats CSF $\text{A}\beta_{42}$ and $\text{A}\beta$ PET as equivalent and interchangeable, a significant number of individuals have shown discordant profiles for the two markers of $\text{A}\beta$.²⁶⁷⁻²⁷⁰ It cannot, therefore, be ruled out that the two biomarkers are capturing slightly different components of $\text{A}\beta$ pathology. To add to this uncertainty, CSF $\text{A}\beta_{42}$ appears not to be a specific biomarker for AD pathology, since CSF $\text{A}\beta_{42}$ reductions have also been observed in other diseases (e.g. Creutzfeldt-Jakob disease, amyotrophic lateral sclerosis, multiple system atrophy).²⁷¹

The development of CSF assays for measuring total and phosphorylated tau levels followed shortly after those for CSF A β ₄₂.^{272,273} Neuropathological studies, however, illustrated that the amount of NFTs detected *post-mortem* correlated only moderately with CSF total tau,²⁷⁴ while the relationship with phosphorylated tau levels was more complex. More specifically, it appears that levels of NFTs correlate with measures of tau phosphorylated at threonine 231²⁷⁵ but not with tau phosphorylated at threonine 181,²⁷⁶ the most common clinical measure of phosphorylated tau. Studies showing correlations of varying strengths between the binding of the newly developed tau-specific PET tracers and CSF tau measures have started to emerge, although doubts have been expressed that the two markers are reflecting the same component of tau pathology.²⁷⁷⁻²⁸⁰

1.9 DIAGNOSTIC ASSESSMENT OF COGNITIVE IMPAIRMENT

Most patients presenting with cognitive complaints will undergo clinical assessment at a primary care unit, according to national guidelines.²⁸¹ In Sweden, as part of the initial, routine assessment, a detailed history is taken from the patient and informant, followed by physical, including neurological, examination, evaluation of the patient's functional capacity to perform activities of daily living and evaluation of the patient's cognitive performance with brief tests (e.g. the MMSE and the clock-drawing tests, as measures of global cognitive and visuospatial, executive performance, respectively). Finally, the patient undergoes blood tests, and structural brain imaging (computed tomography or MRI), for exclusion of other causes of neurological symptoms. If there is uncertainty following the basic assessment or with cognitive complaints by relatively young patients (under the age of 65 yrs), it is advised that the patients are remitted to secondary specialised units for thorough investigation. This could include detailed cognitive assessment performed by a trained neuropsychologist, speech and language assessment by a qualified speech pathologist, electroencephalography, measurements of CSF markers or imaging with different PET tracers (i.e. [¹⁸F]FDG PET or A β PET). The final diagnosis is often based on consensus from a committee composed of geriatricians, neurologists, clinical neuropsychologists, and specialist nurses.

1.10 REVISING THE CLASSICAL DIAGNOSTIC CRITERIA

The development of biomarkers has reconceptualised the diagnosis of AD. In recent years, two sets of different criteria for AD have been published that highlighted the use of biomarkers to identify AD accurately *in vivo*,²⁸²⁻²⁸⁵ even before the onset of dementia, at the preclinical/presymptomatic and prodromal (i.e. MCI due to AD) stages of the disease, in contrast to the classical understanding that AD can only be diagnosed with certainty neuropathologically. Furthermore, these recent AD criteria have suggested that the available biomarkers can be categorised into two groups, based on whether they are specific to the underlying AD pathology (i.e. pathophysiological markers; A β PET and CSF measures for A β ₄₂ and tau) or whether they can track downstream neurodegeneration indicative of the

1.11 TIME COURSE OF THE ALZHEIMER'S DISEASE PATHOLOGY

In the past two decades, a number of researchers have sought to determine the hypothetical time courses of the underlying pathological changes in the brains of patients with AD. The first hypotheses were based on neuropathological studies and highlighted the presence of AD pathology in cognitively normal individuals, thus indicating the preclinical, silent stages of the disease.^{82,83} The development of biomarkers has enabled the multi-modal and longitudinal evaluation *in vivo* of the different pathological processes in AD, and has subsequently led to revised models. These revised models incorporate measures of A β deposition, measures of cognitive impairment, and inflammatory and other markers of the disease.²⁸⁶⁻²⁸⁸ (Figure 13) The incorporation of tau PET tracers in longitudinal, multi-modal cohorts of patients with AD may shed light on the temporal evolution of tau pathology.

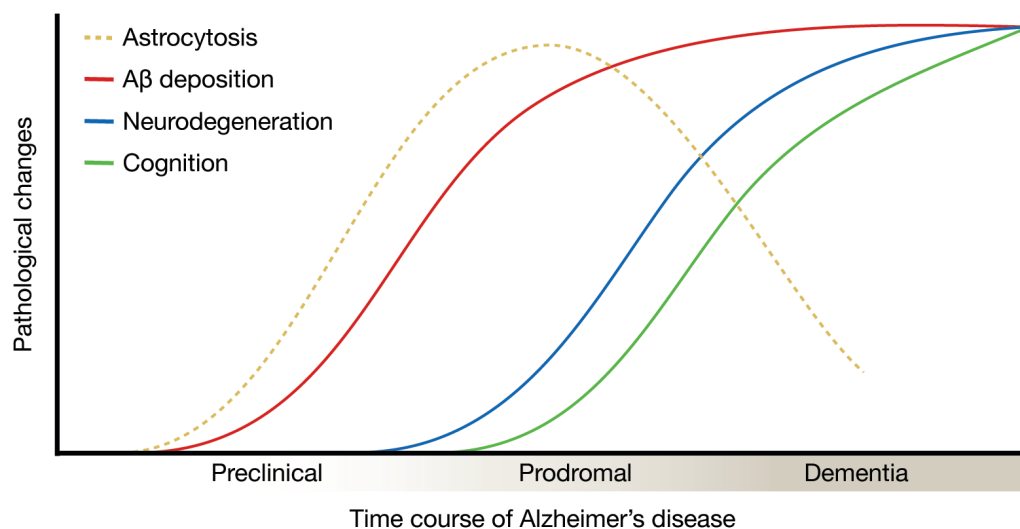


Figure 13. Tentative time course of the pathological changes during the development of AD based on Nordberg, A. Molecular imaging in Alzheimer's disease: new perspectives on biomarkers for early diagnosis and drug development. *Alzheimer's research & therapy* **3**, 34, (2011).

2 AIMS

This thesis aimed with the use of multi-modal PET imaging, to provide new insights on the pathological interplay between tau pathology, neurodegeneration and A β deposition, which underlie the cognitive impairment in AD. The specific aims for each paper were:

In **paper I**, to compare the binding properties of two A β PET tracers ([^{11}C]PIB and [^{18}F]florbetapir) in unrelated but matched patient cohorts, and to examine the effect of age on the distribution of A β -positive scans.

In **paper II**, to evaluate, *in vivo*, the tau-specific PET tracer [^{18}F]THK5317 and to explore the relationship between binding of this tracer and markers of A β deposition ([^{11}C]PIB) and glucose metabolism ([^{18}F]FDG), in a sample of cognitively normal volunteers, patients with clinical diagnosis of AD (prodromal or dementia), and individual patients with atypical parkinsonism.

In **paper III**, to investigate the regional relationship between *in vivo* tau pathology (using [^{18}F]THK5317 PET) and cognitive deficits in a cohort of patients with clinical diagnosis of AD (prodromal or dementia) and to examine the potential role of glucose metabolism ([^{18}F]FDG) as a mediator in this association.

In **paper IV**, to evaluate in a longitudinal multi-modal design the temporal spreading of tau pathology (using [^{18}F]THK5317 PET) in relation to changes in glucose metabolism ([^{18}F]FDG) and cognitive performance in patients with clinical diagnosis of AD (prodromal or dementia) and individual patients with atypical parkinsonism.

In **paper V**, to investigate *in vivo* the binding characteristics of two different tau-specific PET tracers (i.e. [^{11}C]THK5351 and [^{11}C]PBB3) when injected into the same patients with clinical diagnosis of AD (prodromal or dementia); and to explore the relationship between the tracer binding and other markers of the disease.

3 PARTICIPANTS AND METHODS

A thorough description of the participants and the methods applied in each study is presented in the respective articles/manuscripts. Specific methodological aspects are discussed in this section.

3.1 PARTICIPANTS

Different samples of patients and cognitively normal volunteers were included in the different papers. Below is a brief description of the participants in each study.

3.1.1 Paper I

The participants were derived from two multi-centre cohorts of healthy volunteers, patients with MCI and patients with probable AD. The Diagnostic Molecular Imaging (DiMI) consortium was a European-funded project that retrospectively collected, A β PET imaging data from five European centres; the data were analysed centrally with the aim of evaluating the utility of A β PET. The Alzheimer's Disease Neuroimaging Initiative (ADNI) is an on-going USA-based multi-centre study which aims to test whether serial MRI, PET (including A β PET), other biological markers, and clinical and neuropsychological assessment can be combined to measure the progression of MCI and early AD. The data obtained from the ADNI have been organised in an online, open-access database for the research community to use. The patients with MCI and probable AD in both cohorts fulfilled the classical diagnostic criteria.^{14,27,289} We used data from 213 DiMI and 916 ADNI participants, which included a mixture of healthy volunteers, patients with MCI and patients with probable AD. For the comparison with the DiMI cohort, we used an age-, gender-, and MMSE-matched group of participants from the ADNI. For the comparison between age groups, we divided the ADNI sample into two gender- and MMSE-matched groups, based on an age threshold of 75 yrs (n = 363 in each age group).

3.1.2 Papers II-V

All patients included in papers II-V were recruited from the Memory Clinic at the Department of Geriatric Medicine, Karolinska University Hospital, Stockholm, Sweden, after thorough clinical investigation including medical history, physical examination, laboratory blood tests, ApoE genotyping, neuropsychological assessment, CSF sampling and structural imaging. For paper II, 13 patients with MCI, nine with probable AD and two with atypical parkinsonian syndromes (one with possible CBD¹³⁸ and one with probable PSP¹³⁷) were recruited. A subgroup of the patients from paper II was included in the analyses for paper III,

with a smaller subset of the same sample completing a longitudinal follow-up for paper IV. For paper V, a new group of five patients with MCI and four with probable AD were recruited. The diagnosis was based on the consensus of a committee, which included geriatricians, neurologists, clinical neuropsychologists, and specialist nurses. Although all participants were clinically diagnosed according to the classical criteria for MCI and AD,^{14,27} for the purpose of these projects the patients were reclassified based on the new research criteria for AD.²⁸² More specifically, patients with MCI or AD and A β PET or CSF (A β ₄₂ and tau) evidence of AD brain pathology were classified to prodromal AD or AD dementia groups, respectively. According to this classification, for paper I, 11 patients fulfilled the criteria for prodromal AD and nine for AD dementia. For paper V, five participants were classified in the prodromal AD and four in the AD dementia groups.

Nine cognitively normal volunteers (five young and four elderly) were also recruited in paper II for validation purposes. The inclusion criteria for the cognitively normal volunteers included the absence of cognitive complaint, prior head injury, or known neurological/psychiatric disorder. They were all non-smokers and free from medication.

3.2 COMPLIANCE WITH ETHICAL AND REGULATORY STANDARDS

All participants and their caregivers provided written informed consent prior to all investigations and all procedures performed were in accordance with the ethical standards of the institutional and national research committee and with the 1964 Helsinki Declaration and its later amendments, or comparable ethical standards. All studies were approved by the Regional Ethical Review Board in Stockholm, Sweden, and the Radiation Safety committees at the Karolinska University Hospital in Stockholm and the Uppsala University Hospital in Uppsala, Sweden. The study reported in paper V was additionally approved by the Medical Products Agency in Sweden since the protocol included the intravenous injection in patients with a novel PET tracer ([¹¹C]THK5351).

3.3 NEUROPSYCHOLOGICAL ASSESSMENT

All the participants described above underwent extensive neuropsychological assessment, at their respective clinics for the multi-centre studies (DiMI and ADNI) (paper I) or at the Memory Clinic at the Department of Geriatric Medicine, Karolinska University Hospital, Stockholm, Sweden, for the studies included in papers II-V. For papers II-V, the participants underwent baseline assessment, with the participants of the only longitudinal study (paper IV) undergoing additional follow-up neuropsychological evaluation (median interval = 17 months; interquartile range = 15:18).

3.3.1 Paper I

MMSE was selected as a measure of global cognitive function over other more detailed neuropsychological tests because of the wide heterogeneity in the neuropsychological batteries used among the different centres (DiMI) or between the different cohorts (DiMI versus ADNI).

3.3.2 Paper II-V

Global cognition and episodic memory tests were selected to characterise the participants in papers II-V, and to perform regression analyses against PET imaging measures (papers III-V). For the regression analyses, the MMSE and the full-scale intelligence quotient (FSIQ), which is based on five subtests from the Wechsler adult intelligence scale (Similarities, Information, Block Design, Digit Span, and Digit Symbol),²⁹⁰ were used as measures of global cognition. The FSIQ was presented either alone or in relation to the premorbid cognitive function of the individual, as assessed with the irregularly spelled words subtest from the Swedish National Adult Reading Test.²⁹¹ Encoding and delayed recall from the Rey auditory verbal learning test, and delayed recall from the Rey-Osterrieth complex figure test were used for regression analyses for episodic memory (Table 2). The results of all the neuropsychological tests were reported following a z-score transformation for comparison with a reference group of age-matched cognitively normal volunteers.²⁹²

Table 2. Neuropsychological tests used in this thesis for cognitively assessing the participants.

Global cognition	Episodic memory
MMSE	Rey auditory verbal learning; encoding
FSIQ	Rey auditory verbal learning; delayed recall
Decline in FSIQ from premorbid cognitive function	Rey-Osterrieth complex figure; delayed recall

3.4 MULTI-MODAL PET DESIGN

The multi-modal PET design used in all the papers described in this thesis was a powerful tool that enabled the detailed *in vivo* characterisation of different aspects of the AD pathophysiology at the same time point. This approach is based on the injection of different radiotracers on the same day or in close temporal proximity, to the same participant. Apart from the evaluation of different pathophysiological processes, this approach enables the unbiased, direct comparison of different radiotracers in the same individual on the same day, as described in paper V. Tracers with [¹¹C] labelling were preferred for ‘multi-tracer’ imaging

on the same day, because of the very short half-life of the isotope, which allows imaging with two, or even more radiotracers with an interval of just a few hours between injections.

3.4.1 Image acquisitions

3.4.1.1 Paper I

A β PET imaging data were available for all participants from the DiMI and ADNI cohorts, ($[^{11}\text{C}]\text{PIB}$ and $[^{18}\text{F}]\text{florbetapir}$, respectively); $[^{18}\text{F}]\text{FDG}$ imaging data were available only for the ADNI cohort. PET acquisitions were performed on different PET scanners with different protocols for every centre within the different cohorts. A 3D T1 MRI sequence was available for a subset of 151 participants from the DiMI cohort and all 916 ADNI participants.

3.4.1.2 Papers II-IV

All patients in papers II-IV underwent, in close temporal proximity, baseline tau, A β and glucose metabolism PET imaging using $[^{18}\text{F}]\text{THK5317}$, $[^{11}\text{C}]\text{PIB}$ and $[^{18}\text{F}]\text{FDG}$, respectively. The healthy volunteers underwent only tau ($[^{18}\text{F}]\text{THK5317}$) PET imaging, with the exception of the elderly who underwent an additional A β ($[^{11}\text{C}]\text{PIB}$) PET scan to exclude the presence of underlying A β pathology. All participants underwent a 3D T1 MRI sequence at baseline. The patients involved in longitudinal investigations underwent follow-up $[^{18}\text{F}]\text{THK5317}$ and $[^{18}\text{F}]\text{FDG}$ PET imaging scans after a median interval of 17 months (interquartile range = 15:18) (paper IV). All $[^{18}\text{F}]\text{THK5317}$ and $[^{11}\text{C}]\text{PIB}$ PET acquisitions were dynamic (0-60 min) and performed on an ECAT EXACT HR+ scanner (Siemens/CTI) or a Discovery ST PET/CT scanner (GE) at the Uppsala PET centre, Uppsala, Sweden. The $[^{18}\text{F}]\text{FDG}$ PET acquisitions were static (30-45 min) and were performed on a Biograph mCT PET/CT scanner (Siemens) at the Department of Nuclear Medicine, Karolinska University Hospital Huddinge, Stockholm, Sweden.

3.4.1.3 Paper V

All patients in paper V underwent imaging with the tau-specific PET tracers $[^{11}\text{C}]\text{THK5351}$ and $[^{11}\text{C}]\text{PBB3}$ on the same day, as well as with the A β PET tracer $[^{11}\text{C}]\text{AZD2184}$ within a week. All PET acquisitions were dynamic (0-90 min for $[^{11}\text{C}]\text{THK5351}$ and 0-60 min for $[^{11}\text{C}]\text{PBB3}$ and $[^{11}\text{C}]\text{AZD2184}$) and were performed on a high-resolution research tomograph (HRRT, Siemens/CTI) at the Centre for Psychiatry Research, Karolinska Institutet, Stockholm, Sweden. A 3D T1 MRI sequence was also acquired for all patients, within three months from the PET investigations.

3.4.2 Test-retest evaluation

As part of the investigations for paper II, five patients (four with prodromal AD and one with possible CBD) underwent a second PET scan with [^{18}F]THK5317 within one month of the first investigation. This aimed to evaluate, for the first time, the test-retest variability of the tracer.

3.4.3 Image pre-processing

3.4.3.1 Paper I

The [^{11}C]PIB and [^{18}F]florbetapir imaging data were non-linearly spatially normalised to population-specific PET templates in the Montreal Neurological Institute (MNI) space for both tracers (SPM5), where the tracer binding was quantified. The [^{18}F]florbetapir template was based on the procedure previously applied to the [^{11}C]PIB data.^{201,293} Briefly, 207 [^{18}F]florbetapir images were co-registered to their respective T1 MRI sequences, and were later normalised to MNI space using the non-linear transformation matrix from the individual T1 MRI sequence segmentations. An average [^{18}F]florbetapir image was subsequently created and used as a template for the spatial normalisation of all [^{18}F]florbetapir imaging data to MNI space.

3.4.3.2 Papers II-IV

The individual [^{18}F]THK5317, [^{11}C]PIB and [^{18}F]FDG imaging data were co-registered to the individual native T1 MRI sequences (SPM8), where the binding/uptake of the tracers was quantified.

3.4.3.3 Paper V

A different approach was selected for preserving the high-resolution of the PET imaging data in paper V. The T1 MRI sequences of the individual patients were co-registered to the individual [^{11}C]THK5351, [^{11}C]PBB3 and [^{11}C]AZD2184 imaging space (SPM12). The tracer binding was quantified in the native PET space, which was different for each imaging modality.

3.4.4 Quantification of tracer binding

For the regional quantification of the tracer binding/uptake, we employed regions of interest (ROIs) from different brain atlases for each paper, based on the research question and hypothesis.²⁹⁴⁻²⁹⁹ For all studies, in addition to the individual ROIs employed, a composite

isocortical ROI was created to quantify the A β PET data, calculate the cut-offs for A β positivity, and classify the participants in the ‘A β -positive’ and ‘A β -negative’ groups.

3.4.4.1 Paper I

A simplified atlas was used in paper I because of the widespread binding of the A β tracers in the whole isocortex. Grey-matter ROIs, based on the available MRIs from the DiMI cohort,²⁰¹ were created because of the lack of T1 MRI sequences for all of the DiMI cohort, and were later applied to the A β PET scans of all study participants (DiMI and ADNI).

For [^{11}C]PIB and [^{18}F]florbetapir, standardised uptake value ratio (SUVR) images were created (over the time intervals 40-60 min and 50-70 min, respectively), and used to quantify the tracer binding. A cerebellar grey-matter ROI was used as reference for the [^{11}C]PIB images and a whole cerebellar ROI was used for the [^{18}F]florbetapir images.

3.4.4.2 Papers II-V

Grey-matter was parcellated from T1 MRI sequences using SPM (SPM8, SPM12). Grey-matter binary masks were created from this parcellation, and these were later applied to anatomical atlases for the creation of individual grey-matter ROIs. In papers II-III, in which [^{18}F]THK5317 binding was evaluated for the first time *in vivo*, grey-matter ROIs covering the whole brain were applied to all PET tracers. In contrast, for papers IV-V, we selected grey-matter ROIs predominantly in the temporal cortex, in agreement with the findings of papers II-III and the known regional distribution of tau pathology, as described by autopsy studies.^{49,75}

A voxel-wise, reference region-based approach was adopted for the kinetic modelling of the dynamic [^{18}F]THK5317 PET imaging data. The Logan graphical method, with reference to the cerebellar grey-matter ROI, was applied to the dynamic data over the time interval 30-60 min to create the distribution volume ratio (DVR) images, a method that has been validated against arterial sampling-based quantification of the tracer binding.^{227,300} Summation images (40-60 min) were used for [^{11}C]PIB and static images (30-45 min) were used for [^{18}F]FDG to create SUVR images, with reference to the cerebellar grey-matter and pons, respectively. The resulting [^{18}F]THK5317 DVR and [^{11}C]PIB and [^{18}F]FDG SUVR images were sampled with the grey-matter ROIs.

The quantification of the [^{11}C]THK5351, [^{11}C]PBB3 and [^{11}C]AZD2184 dynamic PET imaging binding data was modelled using the wavelet-aided parametric imaging method,³⁰¹ which allows the creation of high-resolution, noise-robust, non-displaceable binding potential (BP_{ND}) images. The cerebellar grey-matter ROI was used as reference for the creation of the BP_{ND} images, which were subsequently sampled with the grey-matter ROIs. The wavelet-

aided parametric imaging method was first compared to other kinetic models for validation purposes.^{226,227,300,302}

3.4.5 Partial volume effect correction

PET is characterised by low spatial resolution and the concentration of a radiotracer might therefore be over- or under-estimated in a given ROI due to potential ‘spill-over’ of the signal from neighbouring ROIs (aka partial volume effect). Different areas of the brain are differentially affected by the partial volume effect; ROIs neighbouring other ROIs that have a different target availability or ROIs with significant atrophy are liable to experience greater spill-over of the signal. Correction methods can be applied based on detailed structural information from the T1 MRI sequence. Specifically, these methods could theoretically compensate for the spill-over of the signal by assuming that different tissue classes in the brain (e.g. grey- and white-matter)³⁰³ or even individual ROIs,³⁰⁴ have a homogeneous signal. Two T1 MRI-based partial volume effect correction methods were applied to the PET data for the purposes of this thesis (papers II, III, V).

3.5 CORTICAL THICKNESS MEASURES

The thickness of the entorhinal cortex was measured for study V, in the T1 MRI sequence, with FreeSurfer image processing software (version 6.0, <http://surfer.nmr.mgh.harvard.edu>). The selection of the entorhinal cortex as a measure of medial temporal atrophy was based on previous evidence of a correlation between the binding of another tau-specific PET tracer ([¹⁸F]AV-1451) with underlying atrophy in the same region.³⁰⁵

3.6 CEREBROSPINAL FLUID BIOMARKERS

As part of the routine clinical assessment, CSF samples from the patients were analysed at the Clinical Neurochemistry Laboratory, Gothenburg University, Mölndal, Sweden. The local reference values of <550 pg/mL for A β ₄₂, >400 pg/mL for total tau, and >80 pg/mL for tau phosphorylated at threonine 181 were used to evaluate the presence of AD pathology in the patients.

3.7 STATISTICAL ANALYSES

Diverse statistical analyses (descriptive and inferential) were used in the respective papers based on the research question and hypothesis. Detailed descriptions of the different approaches used are reported in the respective papers. The approaches to correction for

multiple comparisons are also discussed in the individual papers. For the imaging data, analyses were performed in a ROI- and voxel-based manner, as discussed below.

3.7.1 Region of interest-based analyses

The selection of parametric or non-parametric approaches for group comparisons (analysis of variance or the non-parametric Kruskal-Wallis analogue for analysis of variance) and correlation analyses (Pearson or Spearman rank correlation coefficients) was based on the sample sizes and the probability distributions of the selected variables. To investigate the relationship between imaging modalities or between an imaging modality and other markers of the disease, linear models were constructed for cross-sectional and linear mixed effects models for longitudinal data. Mediation analyses were employed to explore the mediation effect of a variable in the relationship between a causal variable and an outcome variable. Individual annual rates of change in the tracer binding/uptake were calculated, based on the longitudinal data. The expectation-maximisation algorithm for Gaussian mixture models was employed for clustering groups of individuals based on the probability distribution of specific variables. The receiver operating characteristic analysis was used for defining the accuracy of A β and tau PET imaging in discriminating between cognitively normal volunteers and patients with AD, and for selecting optimal cut-off points. For each paper, the ROI-based analyses were performed using different versions of the SPSS (Armonk, New York, USA), XLSTAT (Addinsoft, New York, USA) or R software (R Foundation for Statistical Computing, Vienna, Austria, <http://www.R-project.org/>).

3.7.2 Voxel-based analyses

Group comparisons of the tracer binding were performed using standard non-parametric procedures based on permutation testing (SnPM13), because of the limited sizes of the individual groups. Paired t-tests were employed for investigating changes in the tracer binding/uptake over time (SPM8). Correlation analyses were carried out between the local binding/uptake results for the different tracers (BPM 3.1). Additional procedures included the creation of individual z-score maps for expressing the tracer binding/uptake for an individual in relation to a group of cognitively normal volunteers. The same maps were also assessed longitudinally for exploring the spread of the tracer binding/uptake in individual patients. Maps of the individual annual rates of change were made for the tracer binding/uptake based on the longitudinal data. All voxel-based analyses were performed in MATLAB 2012b (The MathWorks, Inc., Natick, Massachusetts, USA).

4 RESULTS AND REFLECTIONS

More detailed presentation and discussion of the results of each study is included in the respective articles/manuscripts. The main findings as well as some methodological considerations are described briefly below.

4.1 MAIN FINDINGS

4.1.1 Paper I – Amyloid- β PET imaging

4.1.1.1 Comparability of [^{11}C]PIB and [^{18}F]florbetapir PET imaging

The different A β PET tracers have shown similar binding properties when injected into the same participants,¹⁹³⁻¹⁹⁵ although their comparability across different groups was uncertain. In our study, it was observed that the binding of [^{11}C]PIB and [^{18}F]florbetapir, when the tracers were injected into different individuals from different cohorts (DiMI and ADNI, respectively), showed high regional agreement as well as significant correlation across ROIs in the different diagnostic groups, which illustrates the similarities between the tracers (Figure 14). [^{11}C]PIB showed a higher discriminative ability between cognitively normal volunteers and patients with AD than [^{18}F]florbetapir (area under the curve = 0.931 vs 0.864,

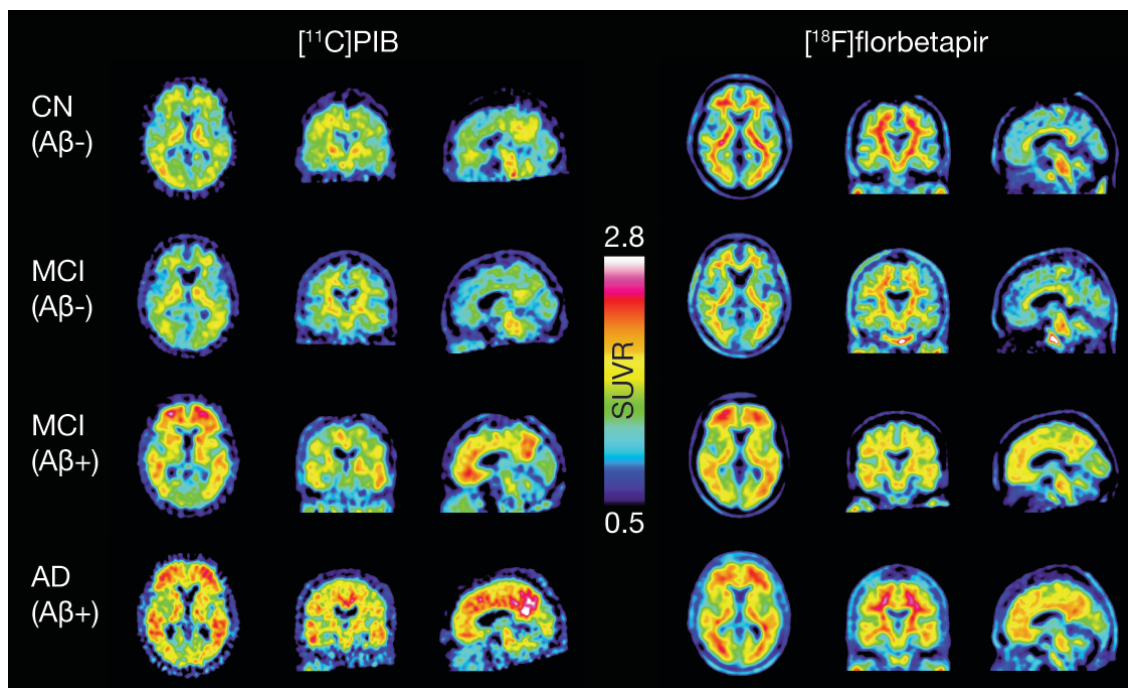


Figure 14. [^{11}C]PIB and [^{18}F]florbetapir SUVR images from age-, gender- and MMSE-matched cognitively normal volunteers (CN), patients with MCI (A β -negative and -positive) and patients with probable AD. The figure is adapted from Chiotis, K. *et al.* Amyloid PET in European and North American cohorts; and exploring age as a limit to clinical use of amyloid imaging. *European journal of nuclear medicine and molecular imaging* **42**, 1492-1506, (2015).

respectively), a finding that had previously been reported elsewhere,¹⁹⁵ although it was not investigated in detail. The wider dynamic range of SUVR values and lower off-target binding in white-matter that is observed for [¹¹C]PIB relatively to its [¹⁸F] derivatives probably contributes to its higher discriminative ability, although it remains unclear if those differences could affect the clinical performance of the [¹⁸F] A β tracers. The differences in discriminative ability between the tracers could alternatively be explained by other differences between the cohorts. Although we used matched groups of individuals, we cannot exclude that other covariates differed. For example, there was a difference in educational attainment between cohorts. The participants in the ADNI cohort were, on average, university graduates, whereas the average educational attainment of the participants in the DiMI cohort was equivalent to high-school graduates. The evidence from the literature suggests differences in the distribution of A β -positive PET scans depending on the educational attainment of the individuals, which could explain the differences in discriminative ability, although this phenomenon is not completely understood, especially among patients with AD.^{196,306-311}

4.1.1.2 Effect of age on the distribution of amyloid- β -positive scans

The rapid development of A β PET imaging led to its approval by the regulatory agencies for clinical use in excluding AD pathology in individuals with cognitive impairment. However, several questions related to the clinical application of A β imaging remain unanswered, including the selection of patients (using demographic or clinical information) that would benefit the most by the incorporation of this expensive imaging technique in their clinical assessment. So far, appropriate use criteria based on the prevalence of different dementia syndromes have suggested that A β imaging should be used in patients younger than 65 years.²⁰⁷ However, little is known on the potential effect of age on the clinical utility of A β imaging in patients with AD, especially across the wide range of ages affected by this disease. In the ADNI participants, we found that A β imaging performed better when discriminating between cognitively normal volunteers and patients with a clinical diagnosis of AD, who were younger (55-75yrs), rather than older (76-93 yrs) (sensitivity = 81 vs 72% and specificity = 70-80%, respectively). While we would expect a drop in specificity due to the age-related accumulation of A β in the population,⁵¹ the drop in sensitivity probably reflected the substantial number of clinically diagnosed patients with AD in the older subgroup who actually did not carry A β pathology. A closer look at the distribution of A β PET measures sheds some light on the uncertain clinical diagnosis of the elderly patients. Specifically, the distribution was bimodal in the elderly patients, with a substantial number of individuals clearly A β -negative (n=15, 22%) (Figure 15). Furthermore, the same patients were less likely to be ApoE4 carriers (one out of 15) and, in general, had a pattern of [¹⁸F]FDG uptake not suggestive of the presence of AD neurodegeneration. Neuropathology studies have pointed in the same direction, and our results were verified by a recent meta-analysis of A β PET imaging data; the prevalence of A β positivity decreases with increasing age in patients with a clinical diagnosis of AD, which indicates an increased clinical misdiagnosis of AD in the

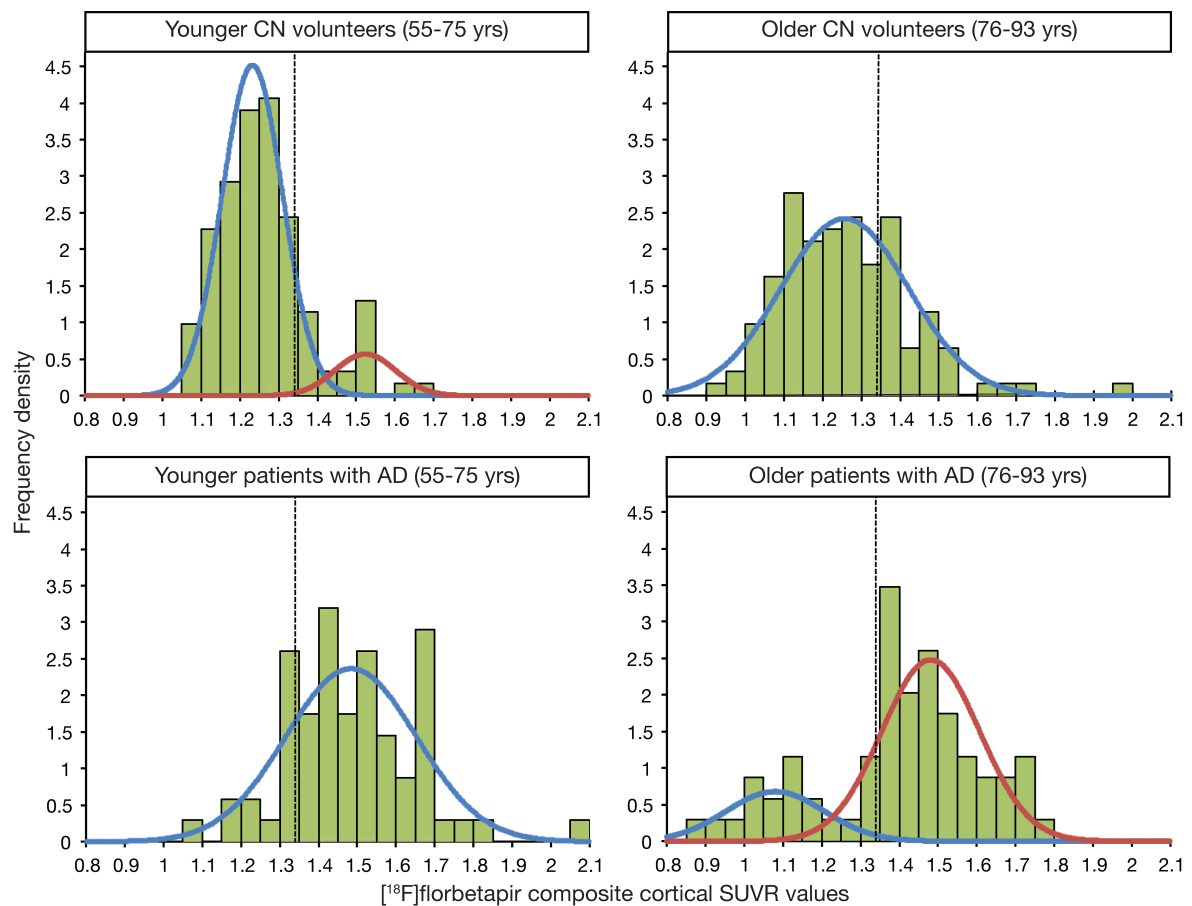


Figure 15. Frequency density plots of the [^{18}F]florbetapir composite cortical SUVR values in the two age groups of cognitively normal volunteers (CN) and patients with probable AD. The dashed line represents the cut-off for A β positivity with [^{18}F]florbetapir. The figure is adapted from Chiotis, K. *et al.* Amyloid PET in European and North American cohorts; and exploring age as a limit to clinical use of amyloid imaging. *European journal of nuclear medicine and molecular imaging* **42**, 1492-1506, (2015).

oldest-old in the absence of a reliable pathology marker.³¹¹ Despite its exploratory nature, this study offers some insight into the increasing importance of A β PET imaging with increasing age in the diagnostic assessment of individuals with cognitive impairment. The ongoing large, multi-centre studies (AMYPAD, IDEAS) that intend to evaluate the clinical performance of A β PET imaging offer a unique opportunity for enhancing our understanding of different clinical measures that could define subgroups of patients, where the use of such a biomarker would be more advantageous.

4.1.2 Papers II-V – Tau PET imaging in a multi-modal design

4.1.2.1 Binding of the tau tracer [^{18}F]THK5317 in patients with AD

The first *in vivo* evaluation of the tau-specific PET tracer [^{18}F]THK5317 in patients with AD (prodromal or dementia) detected high binding of the tracer predominantly in inferior and lateral temporal ROIs, regions that have been consistently associated with the presence of tau pathology in neuropathological studies of AD (Figure 16).^{49,75} In contrast, the cognitively

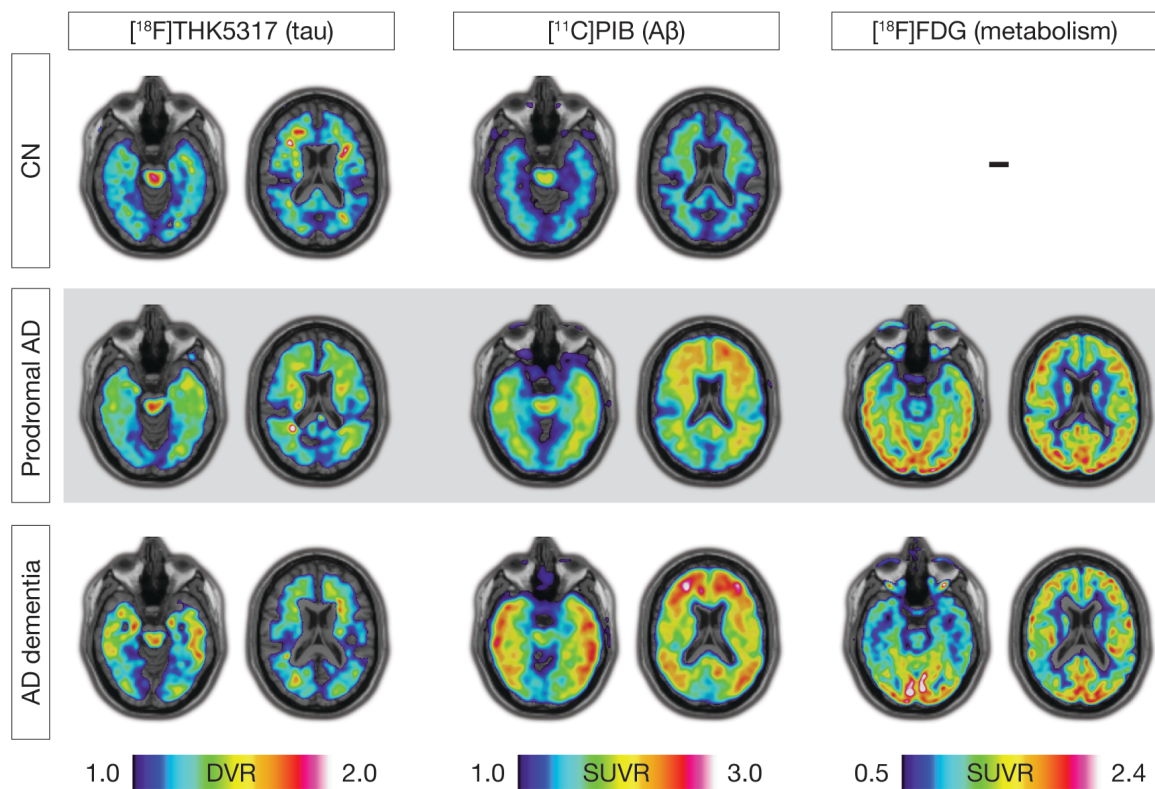


Figure 16. Sample $[^{18}\text{F}]\text{THK5317}$ DVR, $[^{11}\text{C}]\text{PIB}$ SUVR and $[^{18}\text{F}]\text{FDG}$ SUVR images from an elderly cognitively normal (CN) volunteer, a patient with prodromal AD and a patient with AD dementia. Cerebellar grey-matter was used as a reference region for $[^{18}\text{F}]\text{THK5317}$ and $[^{11}\text{C}]\text{PIB}$, and the pons was used for $[^{18}\text{F}]\text{FDG}$.

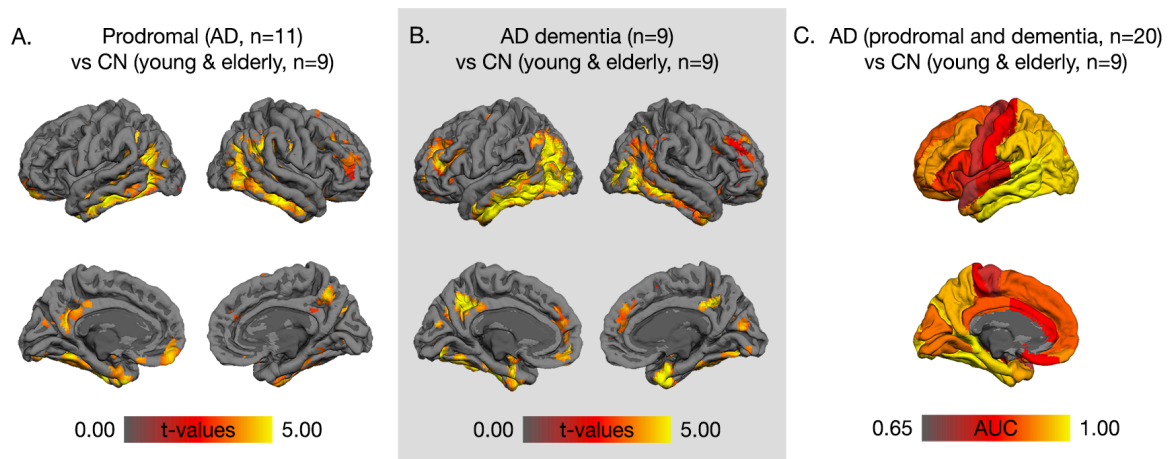


Figure 17. (A, B) Voxel-based group comparisons of $[^{18}\text{F}]\text{THK5317}$ binding between cognitively normal volunteers and patients with prodromal AD or AD dementia; the voxel-based comparisons were performed in SnPM13 and the results are presented after correction for multiple comparisons with the false discovery rate method ($p < 0.05$). (C) ROI-based receiver operating characteristic analysis between all cognitively normal volunteers and all patients with AD (prodromal and dementia). The area under the curve (AUC) for every cortical ROI was reported. The figure is adapted from Chiotis, K. *et al.* Imaging in-vivo tau pathology in Alzheimer's disease with THK5317 PET in a multimodal paradigm. *European journal of nuclear medicine and molecular imaging* **43**, 1686-1699, (2016).

normal volunteers showed overall low binding of the tracer, with areas of high binding limited to the basal ganglia. Statistically significant differences were observed between patients with AD and cognitively normal volunteers predominantly in the temporal lobe as well as in other isocortical ROIs (Figure 17A, B). Furthermore, the ordering of ROIs with regard to discrimination between groups strongly resembled the suggested temporal evolution of tau pathology across the AD brain (Figure 17C),⁷⁵ in agreement with another study that used the same methodology but a different tau tracer (i.e. [^{18}F]AV-1451).²³³ The findings of this study, together with *in vitro* evidence highlighting the specificity of this tracer for tau deposits,²¹⁸ suggest that [^{18}F]THK5317 could image the expected load and regional pattern of tau pathology *in vivo* in a cohort of cognitively normal volunteers and patients with AD. Similar findings have been reported in different cohorts, where different tau-specific PET tracers were used.^{220,312}

The binding pattern of [^{18}F]THK5317 in patients with AD differed from that of the A β PET tracer [^{11}C]PIB (Figure 16), which further illustrates the differences between the targets of the two tracers. However, there were regional correlations between the two markers (Figure 18A), which may reflect the co-localisation of A β and tau deposits during the time course of AD, probably in the neuritic plaques. Similar findings have been reported for the tau PET tracer [^{18}F]AV1451.²⁴³ Significant correlations between [^{18}F]THK5317 and neurodegeneration, as measured by glucose hypometabolism ([^{18}F]FDG), were regionally localised in areas vulnerable to neurodegeneration in the fronto-parieto-temporal lobes, including the precuneus, highlighting the close link between tau pathology and neurodegenerative changes (Figure 18B).⁶⁵⁻⁶⁸ However, in contrast to other studies published with another tracer, the relationship between the tracer binding and the neurodegenerative changes was rather focal and did not occur across large cortical areas,^{237,240,242} which could

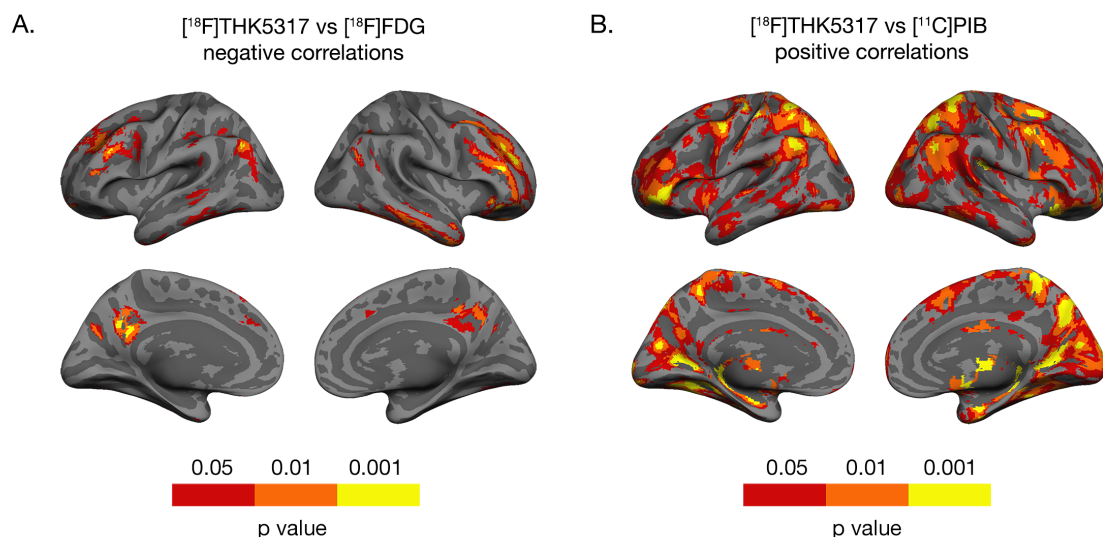


Figure 18. Voxel-based correlations between (A) [^{18}F]THK5317 (tau) and [^{11}C]PIB (A β) binding and (B) [^{18}F]THK5317 (tau) binding and [^{18}F]FDG (glucose metabolism) uptake. The correlation analyses were performed in BPM 3.1. No correction for multiple comparisons was applied. The figure is adapted from Chiotis, K. *et al.* Imaging in-vivo tau pathology in Alzheimer's disease with THK5317 PET in a multimodal paradigm. *European journal of nuclear medicine and molecular imaging* **43**, 1686-1699, (2016).

be attributed to our mildly impaired sample, where only a subset of patients had severe hypometabolic changes.

4.1.2.2 Relationship of tau pathology ($[^{18}\text{F}]\text{THK5317}$) with cognitive deficits

Binding of $[^{18}\text{F}]\text{THK5317}$ in patients with AD related negatively to measures of global cognition (MMSE, FSIQ) and episodic memory (encoding from the Rey auditory verbal learning and delayed recall from the Rey-Osterrieth complex figure tests) (Figure 19). The correlations, especially that with episodic memory, were predominantly observed in the temporal lobe, where the patients showed increased binding in comparison to a group of cognitively normal volunteers. Widespread hypometabolism ($[^{18}\text{F}]\text{FDG}$) in fronto-parieto-temporal areas related positively with measures of global cognition, while the relationship with episodic memory was somewhat more restricted spatially in comparison to

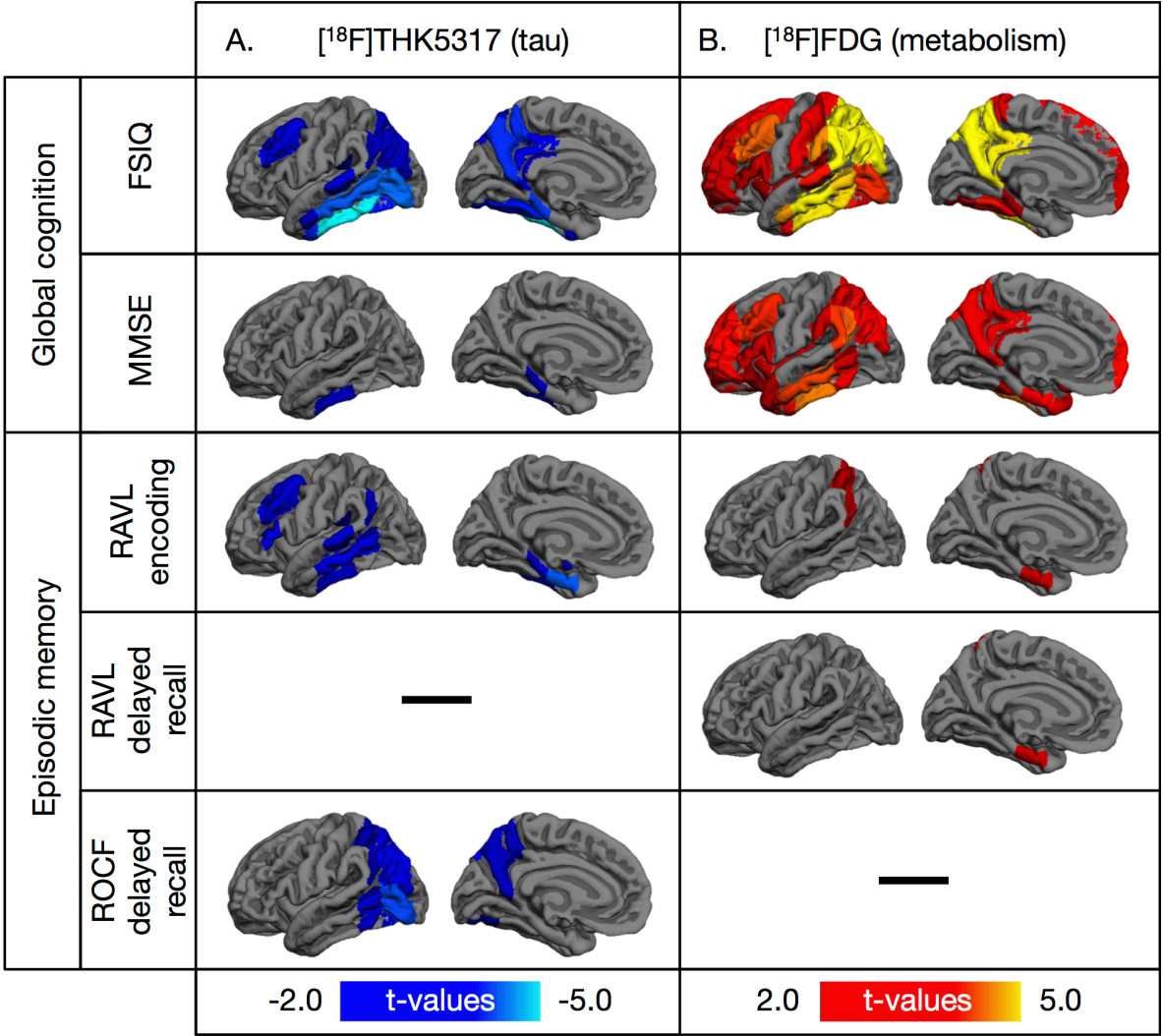


Figure 19. Surface projections describing the relationship of ROI-based tracer binding/uptake ($[^{18}\text{F}]\text{THK5317}$ and $[^{18}\text{F}]\text{FDG}$) with global cognitive and episodic memory performance in patients with AD. Linear models were employed for investigating relationships with t-values reported for significant associations ($p<0.05$). No correction for multiple comparisons was made. RAVL = Rey auditory verbal learning; ROCF = Rey-Osterrieth complex figure. The figure is adapted from Saint-Aubert, L. *et al.* Regional tau deposition measured by $[^{18}\text{F}]\text{THK5317}$ positron emission tomography is associated to cognition via glucose metabolism in Alzheimer's disease. *Alzheimer's research & therapy* **8**, 38, (2016)

[¹⁸F]THK5317. From our evidence, tau pathology, relatively to glucose metabolism, seems to be more selective for episodic memory changes, while the opposite pattern was observed for global cognition. Similar correlations have been observed between the binding of other tau tracers and cognition in different patient samples.^{231,234,237,313}

Based on current understanding, tau deposition could lead to neuronal dysfunction, neuronal death and finally cognitive deficits.^{55,69-71} In order to test this hypothesis *in vivo*, we used mediation analyses to investigate possible causal relationships between tau deposition ([¹⁸F]THK5317), glucose metabolism ([¹⁸F]FDG) and cognition. Briefly, the prerequisite for those analyses was the presence of a statistically significant relationship of the mediator variable (glucose metabolism) with the other two variables (tau deposition and cognition). This condition was met for [¹⁸F]THK5317 and [¹⁸F]FDG binding/uptake in the ROIs of the temporal lobe and measures of global cognition. A mediating role of [¹⁸F]FDG uptake was detected in the association of local [¹⁸F]THK5317 binding with global cognitive measures. Thus, our cross-sectional data support the current hypothesis, according to which increased tau deposition leads to cognitive decline by causing local neuronal dysfunction (hypometabolism). Our findings are in line with those from another study, which incorporated CSF measures instead of PET imaging to trace tau pathology,³¹⁴ although the strength of our current work is the regional mapping of the pathological changes in the AD brain. A study published recently by Bejanin, et al.³¹⁵ further validates our observations by applying similar models with another tau tracer ([¹⁸F]AV-1451).

4.1.2.3 Propagation of tau pathology ([¹⁸F]THK5317) in a longitudinal design

Based on neuropathological evidence, it has been suggested that the regional spreading of tau pathology follows the clinical progression of AD in patients;^{51,77,78} however, no longitudinal tau PET imaging study had been published, which validated these cross-sectional, *post-mortem* observations. In our study, we used a longitudinal design to investigate the temporal evolution (interval = 17 months) of tau pathology *in vivo* using PET ([¹⁸F]THK5317) in relation to changes in glucose metabolism ([¹⁸F]FDG) and cognitive performance in a group of patients with AD (prodromal or dementia). At a group level, no statistically significant increases in [¹⁸F]THK5317 binding were observed over time (except for a restricted unilateral area in the left inferior temporal gyrus), while [¹⁸F]FDG uptake declined significantly in widespread temporo-parietal areas (Figures 20, 21). In temporal ROIs, a statistically significant negative correlation was observed between baseline [¹⁸F]THK5317 binding and annual rates of change of [¹⁸F]THK5317 binding, which illustrates that the rate of tau deposition could even decelerate over time in ROIs with high tau burden at baseline. At an individual level, a heterogeneous pattern of increases in [¹⁸F]THK5317 binding was observed, with differences observed between patients at different clinical stages of AD (prodromal or dementia). Binding was increased in more restricted isocortical areas in patients with prodromal AD in comparison to patients with AD dementia. This illustrates that, although no statistically significant differences were detected at a group level, there were

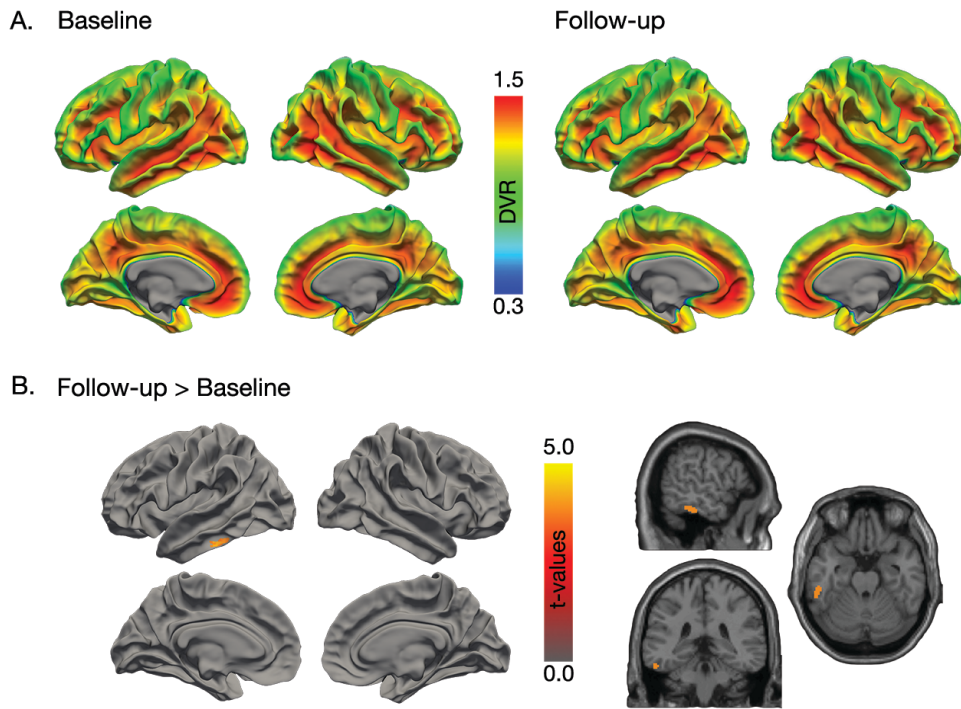


Figure 20. (A) Average baseline and follow-up DVR images from patients with AD (prodromal or dementia; $n=16$) with $[^{18}\text{F}]\text{THK5317}$, and (B) voxel-based paired t-tests (SPM8) evaluating the changes in binding over time (interval = 17 months). No correction for multiple comparisons was made (uncorrected $p<0.001$). The figure is adapted from Chiotis, K. *et al.* Longitudinal changes of tau PET imaging in relation to hypometabolism in prodromal and Alzheimer's disease dementia. *Molecular psychiatry*, (2017).

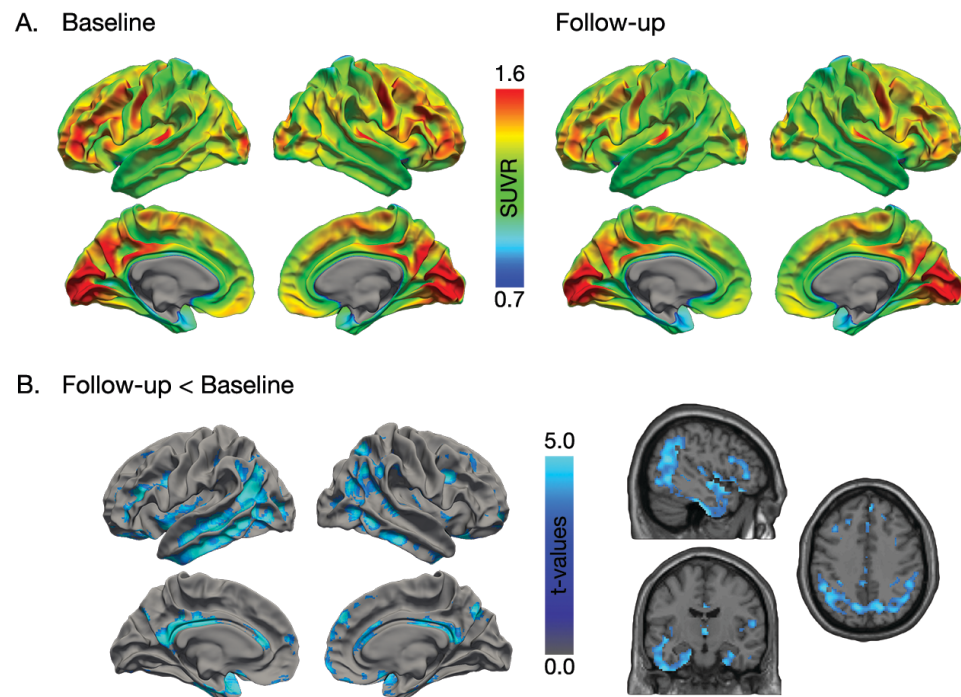


Figure 21. (A) Average baseline and follow-up SUVR images from patients with AD (prodromal or dementia; $n=16$) with $[^{18}\text{F}]\text{FDG}$, and (B) voxel-based paired t-tests (SPM8) evaluating the changes in uptake over time (interval = 17 months). No correction for multiple comparisons was made (uncorrected $p<0.001$). The figure is adapted from Chiotis, K. *et al.* Longitudinal changes of tau PET imaging in relation to hypometabolism in prodromal and Alzheimer's disease dementia. *Molecular psychiatry*, (2017).

substantial albeit heterogeneous differences at an individual level. Similar heterogeneity was also observed, in terms of [^{18}F]THK5317 binding, at baseline in our patient sample.

Longitudinally, no relationship was observed between [^{18}F]THK5317 binding and [^{18}F]FDG uptake in the patients with AD, as assessed by linear mixed-effects models. However, a significant interaction was detected between [^{18}F]THK5317 binding and the time points of investigations (baseline and follow-up) with regard to the [^{18}F]FDG uptake. Specifically, at follow-up the relationship between [^{18}F]THK5317 binding and [^{18}F]FDG uptake was closer than at baseline. In other words, although tau pathology and hypometabolism do not seem to go hand-in-hand over time, the relationship becomes closer as the disease progresses, i.e. as hypometabolism becomes more severe. Cross-sectional *in vivo* observations with another tau tracer ([^{18}F]AV-1451) in samples of patients at different stages of the disease, further supported the idea of a closer relationship between tau pathology and neurodegeneration at late symptomatic stages of AD (dementia).^{240,242,246,316} Altogether, our findings indicate the existence of a lag phase between the build-up of tau pathology and the development of hypometabolic, neurodegenerative changes. This is in line with some experimental data showing that neurons can tolerate a substantial amount of tau pathology, through compensatory mechanisms, before exhibiting major degenerative changes.⁷²⁻⁷⁴

4.1.2.4 Binding of the tau tracer [^{18}F]THK5317 in patients with atypical parkinsonism

A neuropathological diagnosis of CBD and PSP is made in the presence of tau-positive deposits, although distinct types and regional distributions of the deposits characterise the two diseases (Table 2).^{317,318} Both diseases have been associated with clinical symptomatology in the spectrum of atypical parkinsonism with broad overlap between their clinical presentations. Two patients clinically diagnosed with possible CBD and one with probable PSP underwent multi-modal PET imaging as part of our studies (paper II, IV). All three patients were negative for A β deposition ([^{11}C]PIB PET), they exhibited hypometabolic changes ([^{18}F]FDG PET) consistent with the presence of CBD and PSP pathology, respectively, and the regional distribution of their [^{18}F]THK5317 binding differed substantially from that in patients with AD. [^{18}F]THK5317 binding was higher in the two patients with possible CBD than in the cognitively normal volunteers, in areas consistent with the expected distribution of tau pathology in this disease;¹³⁵ both patients showed increased binding in the basal ganglia and cortical areas, while one of the them also showed extensive binding in the white-matter (Figure 22). The patient with probable PSP showed high [^{18}F]THK5317 binding, predominantly in the basal ganglia and midbrain, in agreement with previously published neuropathological studies.¹³⁶ Our findings are in line with evidence presented using different tau PET tracers,^{220,247-252} and illustrate the promise held by the existing tracers for differentiating between syndromes associated with different tauopathies.

The two patients with possible CBD underwent follow-up [^{18}F]THK5317 and [^{18}F]FDG PET imaging after intervals of 17 and 24 months. At follow-up, [^{18}F]THK5317 binding in both

patients had increased in the basal ganglia as well as other cortical areas, including the frontal lobe (Figure 22). Decreases were observed in [^{18}F]FDG uptake over this time. Tau imaging with [^{18}F]THK5317 could thus prove more useful in tracking neurodegeneration longitudinally in non-AD rather than AD tauopathies, at least in the symptomatic stages of these diseases. However, because only two cases of possible CBD were investigated, without autopsy validation, we advise caution in the interpretation of our findings.

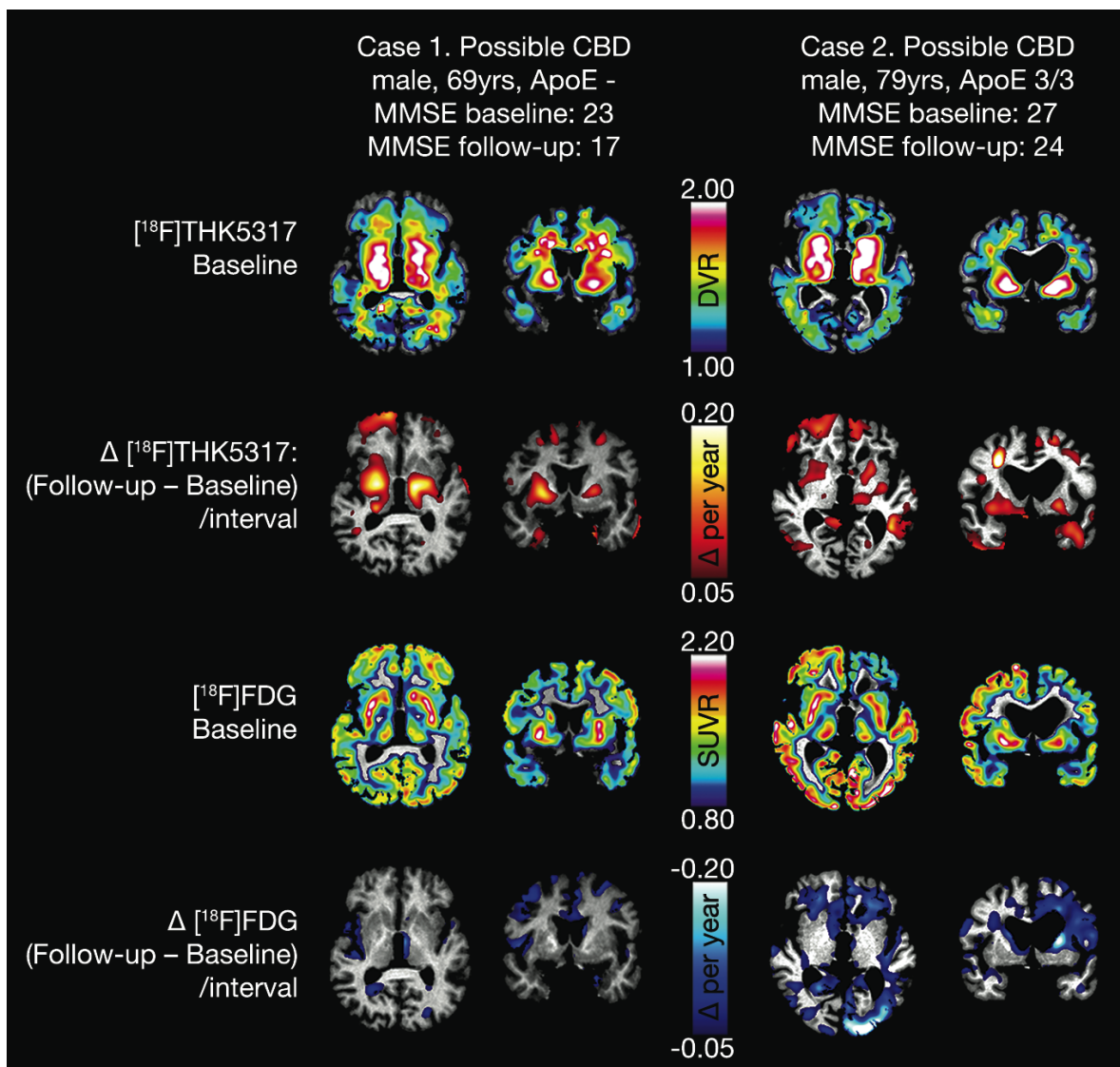


Figure 22. [^{18}F]THK5317 DVR and [^{18}F]FDG SUVR baseline images as well as annual rate of change maps (Δ DVR/SUVR per year) for the binding/uptake of the two tracers in the two patients with clinical diagnosis of possible CBD. The figure is adapted from Chiotis, K. *et al.* Longitudinal changes of tau PET imaging in relation to hypometabolism in prodromal and Alzheimer's disease dementia. *Molecular psychiatry*, (2017).

4.1.2.5 Differences between tau-specific tracers; relationship to other markers of AD

Similar findings have been presented *in vivo* when chemically different tau PET tracers were administered to different patients with AD or non-AD tauopathies, as discussed above.²²³ However, head-to-head comparisons of those tracers in the same individuals were lacking. In our study, the tau tracers [^{11}C]THK5351 (successor of THK5317) and [^{11}C]PBB3 were injected on the same day into the same patients, who were diagnosed with clinical AD (prodromal or dementia), to compare their binding properties. [^{11}C]THK5351 bound with a higher load in the brains of the patients, than [^{11}C]PBB3, with both tracers exhibiting high binding in the temporal lobe, as well as other isocortical ROIs (Figure 23). However, the regional distribution of [^{11}C]THK5351 and [^{11}C]PBB3 binding differed substantially, especially within the temporal lobe. More specifically, while [^{11}C]THK5351 showed the highest binding in the medial relative to the lateral temporal lobe, the opposite pattern was detected for [^{11}C]PBB3. The binding of [^{11}C]PBB3, but not of [^{11}C]THK5351, resembled that of the A β tracer [^{11}C]AZD2184 in the temporal lobe and strong positive correlations were observed between the binding of [^{11}C]PBB3 and [^{11}C]AZD2184. Measures of tau in the CSF, and downstream markers of AD such as entorhinal cortex atrophy and global cognitive performance were more closely related to the binding of [^{11}C]THK5351, than to that of [^{11}C]PBB3. The differences in the load and regional distribution of the binding suggest different molecular targets for the two tau PET tracers. The correlations of the [^{11}C]PBB3 binding with the binding of the A β tracer, suggest that [^{11}C]PBB3 could bind preferentially to tau deposits co-localised with A β pathology (i.e. neuritic plaques).^{319,320} In contrast, the

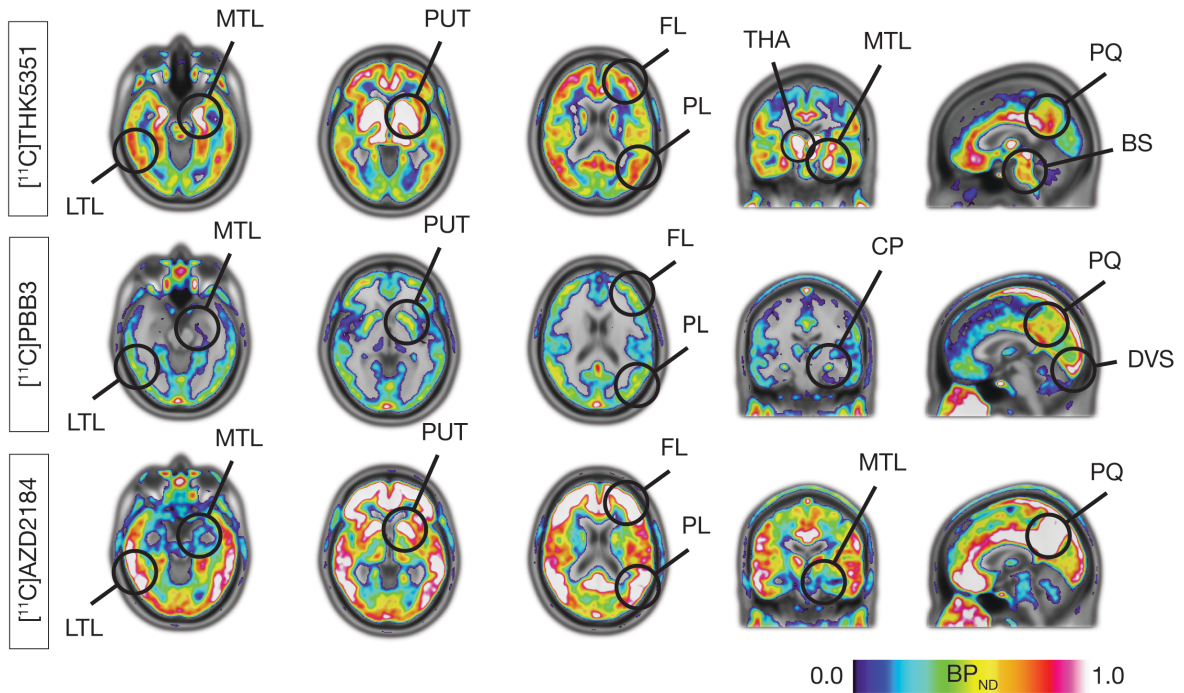


Figure 23. Average [^{11}C]THK5351 (tau), [^{11}C]PBB3 (tau) and [^{11}C]AZD2184 (A β) BP_{ND} images for the patients with AD (prodromal or dementia; $n = 9$). BS = brainstem; CP = choroid plexus; DVS = dural venous sinus; FL = frontal lobe; LTL = lateral temporal lobe; MTL = medial temporal lobe; PQ = precuneus; PL = parietal lobe; PUT = putamen; THA = thalamus.

pattern of [^{11}C]THK5351 binding matched the expected spatial distribution of tau pathology in AD better, suggesting binding of the tracer to a wider range of tau deposits.^{75,321}

4.2 METHODOLOGICAL CONSIDERATIONS

4.2.1 Tau PET imaging

4.2.1.1 Test-retest evaluation

Test-retest studies are crucial in the *in vivo* evaluation of the utility of novel tracers. [^{18}F]THK5317, when injected into the same patients within an interval of 37 days, showed excellent reproducibility, especially in regions of particular interest for tau pathology. In the temporal cortex, the average absolute difference in [^{18}F]THK5317 binding between test and retest was 1.83% (standard deviation = 1.00%). Low variability was also observed in ROIs considered affected by ‘off-target’ binding of the tracer, as discussed below. As an example, the average absolute difference in [^{18}F]THK5317 binding in the putamen between test and retest was 1.51% (standard deviation = 1.07%).

4.2.1.2 Off-target binding

The binding of [^{18}F]THK5317 and its successor [^{11}C]THK5351 was extensive in areas that are not expected to be affected significantly by tau pathology (likely, off-target binding) in cognitively normal volunteers or patients with early AD,⁴⁹ such as the basal ganglia, thalami and brainstem (Figures 23, 24). Binding in the basal ganglia appeared to be of higher intensity in the elderly compared with younger, cognitively normal volunteers, although there was very good discrimination in the same area between groups of cognitively normal volunteers and patients with AD (prodromal or dementia) or atypical parkinsonism. Off-target binding in the basal ganglia and thalami has been associated with binding of the tracer to monoamine oxidase B (MAO-B).²³⁶ Although, the discrimination between patients with atypical parkinsonism and cognitively normal volunteers could indicate a tau component in the binding in those areas, the source of increased binding in patients with AD remains unexplored. Interestingly, the structurally different tau tracer [^{11}C]PBB3 was also

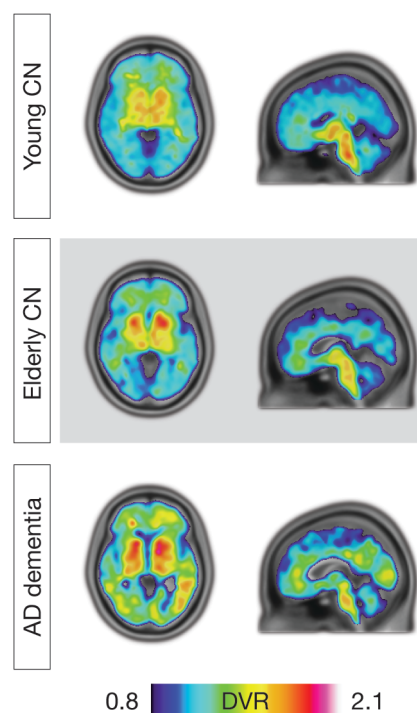


Figure 24. Sample [^{18}F]THK5317 DVR images illustrating the off-target binding of the tracer in areas such as the basal ganglia, thalamus and brainstem from a young cognitively normal (CN) volunteer (22 yrs), an elderly CN (58 yrs) and a patient with AD of the same age (58 yrs).

bound extensively to the MAO-B-rich basal ganglia in patients with AD, although the comparability of off-target binding sources between tracers remains elusive. Additional areas of off-target binding for [^{11}C]PBB3 were detected in vascular structures, including the choroid plexus and the dural venous sinuses (Figure 23).

4.2.1.3 Partial volume effect correction

The extensive off-target binding of the investigated tau tracers could potentially lead to spill-over of the signal to the adjacent ROIs, especially when conventional PET scanners with low spatial resolution (e.g. ECAT EXACT HR+ scanner and Discovery ST PET/CT) are used. We used different methods to correct for this partial volume effect. In the uncorrected [^{18}F]THK5317 DVR images no differences were observed in the hippocampus between the cognitively normal volunteers and patients with AD, possibly because of off-target tracer binding in the basal ganglia, which led to spill-over of signal. Application of partial volume effect correction accounted for the spill-over and revealed that the groups could be differentiated moderately well based on the load of tracer binding (Figure 25). A similar effect was observed in the anterior cingulate. For [^{11}C]THK5351 and [^{11}C]PBB3, the partial volume effect correction did not substantially affect the quantification of the tracer binding, probably because of the high-resolution of the PET system (HHRT), which minimised the spill-over between ROIs. However, it appears that the use of these tracers in conventional scanners would result in substantial spill-over of the signal and therefore bias in the regional quantification of the tracer binding.

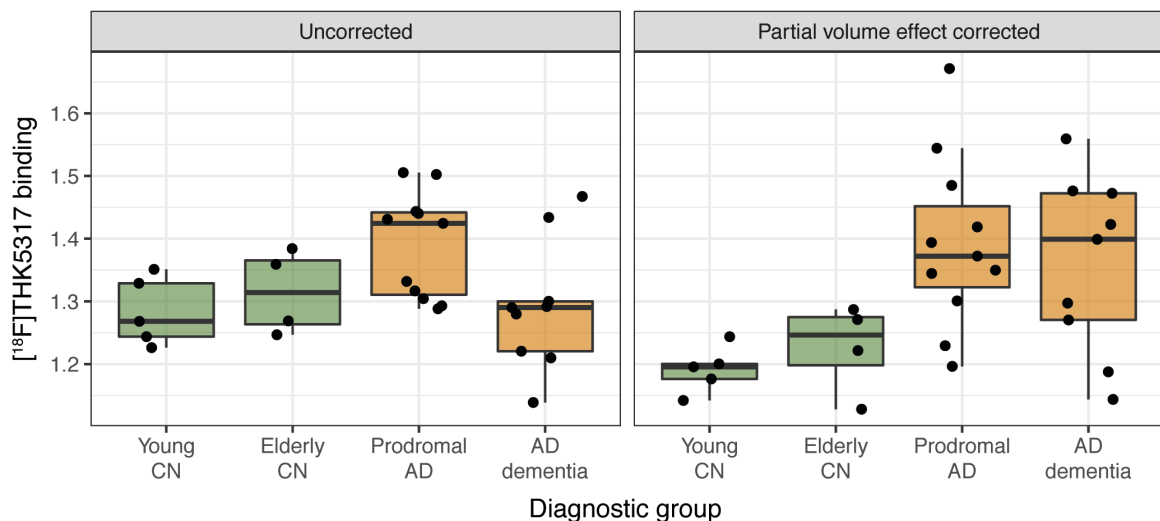


Figure 25. Boxplots of [^{18}F]THK5317 binding in the hippocampus before and after the application of partial volume effect correction across diagnostic groups. CN = cognitively normal volunteers. The figure is adapted from Chiotis, K. *et al.* Imaging in-vivo tau pathology in Alzheimer's disease with THK5317 PET in a multimodal paradigm. *European journal of nuclear medicine and molecular imaging* **43**, 1686-1699, (2016).

5 CONCLUDING REMARKS

- The developed A β -specific PET tracers, [^{11}C]PIB and [^{18}F]florbetapir, were highly comparable even when applied to different cohorts. The oldest old patients with cognitive complaints might benefit substantially from the use of A β PET as part of their clinical assessment.
- The tracer [^{18}F]THK5317 detected the expected load and regional distribution of tau pathology *in vivo* in a sample of patients with clinical AD (prodromal or dementia) and patients with atypical parkinsonism. The distribution of [^{18}F]THK5317 binding differed from that of A β deposition ([^{11}C]PIB) in AD, although there were regional correlations.
- The regional load of tau pathology ([^{18}F]THK5317) is associated with measures of global cognition and episodic memory. Local hypometabolism ([^{18}F]FDG) appeared to play a mediating role in this relationship.
- Heterogeneous patterns of change over time were observed in the binding of the tau tracer [^{18}F]THK5317 in patients with AD, in contrast to homogeneous changes in glucose metabolism ([^{18}F]FDG), which tracked cognitive deterioration better. The build-up of tau pathology and the development of local hypometabolism appeared temporally dissociated, at early symptomatic stages of AD, with a stronger relationship detected when hypometabolism changes become more prevalent in the later stages.
- The tau tracers [^{11}C]THK5351 and [^{11}C]PBB3 seem to bind to different molecular targets *in vivo*. Binding of [^{11}C]PBB3 appeared to be more closely related to A β deposition ([^{11}C]AZD2184), while [^{11}C]THK5351 binding followed the expected regional pattern of tau pathology in AD more closely and was more closely related to downstream markers of the disease.

6 FURTHER CONSIDERATIONS

Although the results of tau PET imaging are promising, a number of concerns have also been raised, predominantly related to the lack of thorough characterisation of the binding targets for each tracer, as discussed below. Therefore, caution is advised in interpreting the *in vivo* findings published to date. Future research should focus on validating the binding of the existing PET tracers as well as on developing new tracers with improved pharmacological properties, based on the lessons learned from the evaluation of the first generation of tracers.

6.1 SPECIFIC TARGETS OF TAU PET TRACERS

The specific targets of the developed tau PET tracers remain uncertain. Although all tracers have shown high specificity to tau pathology in *in vitro* studies,²²³ the heterogeneity of tau deposits complicates the identification of their specific targets, in the absence of detailed validation studies. Furthermore, the differences in chemical structure of the existing tracers raise doubts about the comparability of their binding properties on the tau deposits. To date, studies directly comparing the *in vitro* binding of the tracers have highlighted differences in their binding characteristics. The tracers in the THK family (THK5317, THK5351) and AV-1451 appear to have similar binding properties in the AD brain while PBB3 has different properties, as illustrated by competition studies.^{224,225} These observations have been reinforced by *in vivo* comparisons in the same patients with different tracers, both in paper V and the work of Jang, et al.³²². Therefore, although we know very little about the specific targets of these tracers, we now understand that at least one of them (PBB3) binds to different molecular sites from the rather similar targets that THK5317, THK5351 and AV-1451 bind to. The identification of tracers binding to different aspects of tau pathology may have important implications for the differentiation of tauopathies, as well as for exploration of the temporal evolution of tau pathology in the diseased brain.

The determination of the 3D molecular structure of paired helical and straight tau filaments³²³ could offer new insight into the development of future tau PET tracers. The use of computational simulation studies (*in silico* modelling) will allow detailed investigation of the tracer binding sites on the tau fibril in greater detail, as well as allow determination of whether the tracers preferentially bind to different types of tau filaments. In addition, more detailed characterisation of the tracer binding is expected with the *post-mortem* validation of tracer binding in end-of-life patients. These studies will reveal whether the tracers bind to different types of tau deposits or even to different maturation stages of these deposits. The elucidation of the binding characteristics is crucial for interpreting *in vivo* PET observations in both AD and non-AD tauopathies.

6.2 OFF-TARGET BINDING OF TAU PET TRACERS

The *in vivo* binding of the developed tracers to areas not expected to be affected by tau pathology, both in cognitively normal volunteers and patient groups was somehow largely neglected in the first *in vivo* studies,^{219,220,231,324} probably as a result of the commercial interests surrounding the development of many of the tau-specific tracers. Briefly, recent studies have suggested off-target binding for the tracers to misfolded proteins other than tau (e.g. TDP-43, α -synuclein, A β), enzymes (e.g. MAO-A, MAO-B), and vascular structures.

6.2.1.1 Misfolded proteins

The preliminary evidence pointing to binding of tau tracers to misfolded proteins other than tau^{257,258,325-328} has led to the ‘tau-specificity’ of these tracers being questioned. So far, PBB3 appears to have affinity for α -synuclein, the tracers of the THK family and AV-1451 show high binding *in vivo* in syndromes associated with TDP-43 pathology, and the THK tracer family could have some affinity for A β deposits, according to *in vitro* work. While the latter observations remain to be validated in *ante-/post-mortem* studies, concerns have been raised that these tracers might bind *in vivo* to multiple β -sheet structures (‘amyloids’), although with a different affinity from that to tau pathology. If this proves to be the case, the clinical utility of the developed tracers would be undermined, since the discrimination between different neurodegenerative diseases characterised by the accumulation of misfolded proteins (aka proteinopathies) would be at least questionable.

6.2.1.2 Monoamine oxidase B

Extensive binding in the basal ganglia has been reported *in vivo* for AV-1451 and tracers of the THK family, in both cognitively normal volunteers and patients with AD.^{250,329} However, the basal ganglia are minimally affected by tau pathology in both normal ageing and the early stages of AD.⁴⁹ The binding of the THK tracers to the basal ganglia has been attributed to off-target binding to MAO-B,²³⁶ a finding that is consistent with the regional distribution of MAO-B in the brain.³³⁰ However, a study that attempted to block the MAO-B signal *in vivo* by administering a MAO-B inhibitor prior to the THK5351 PET scan detected decreases in the signal compared to a baseline THK5351 investigation, irrespective of the cerebral distribution of MAO-B. Surprisingly, when the binding was quantified using a conventional reference region-based approach, no differences were noted in terms of binding before and after the administration of the inhibitor. This apparent discrepancy could derive from changes in the perfusion of the tracer following administration of a MAO-B inhibitor. In other words, the MAO-B inhibitor could lead to decreased delivery of the tracer across the whole brain, possibly through nitric oxide-mediated vasodilation,³³¹ which could mask small differences in the binding of THK5351 before and after administration of the inhibitor. Given the very strong correlation between AV-1451 and tracers of the THK family in the basal ganglia when

injected in the same patients,³²² it is conceivable that the source of off-target binding is – at least partly – similar for these tracers. Interestingly, as illustrated in paper V, PBB3 also binds *in vivo* to the MAO-B-rich basal ganglia. Altogether, the potential binding of chemically different tau tracers to the same off-target site might indicate the existence of similarities between binding sites on tau pathology and MAO-B. Detailed validation studies are required to determine the contribution of MAO-B in the *in vivo* signal of the developed tau tracers and to define the brain areas that are affected the most. Potential binding of the tracers to MAO-B has increased relevance in non-AD tauopathies, such as CBD and PSP, where ROIs with high MAO-B availability and tau pathology overlap (e.g. basal ganglia).

6.2.1.3 Vascular structures

AV-1451 and PBB3 both bind to vascular structures, which could complicate the quantification of the tracer binding in multiple ROIs. The source of this binding for AV-1451 has so far been attributed to multiple causes,^{217,259,332} with no studies investigating further this issue for PBB3.

7 FUTURE OUTLOOK

The use of tau PET imaging for ever larger cohorts of patients with AD and non-AD tauopathies, and for cognitively normal elderly, could offer valuable insight on the temporal evolution of tau pathology in the diseased brain, as well as offering a useful tool for the differential diagnosis of different proteinopathies.

7.1 TEMPORAL EVOLUTION OF TAU PATHOLOGY

Tau PET *in vivo* studies with [¹⁸F]THK5317, [¹⁸F]THK5351 and [¹⁸F]AV-1451 have indicated that lateral temporal cortical areas are already affected by tau deposition in the earliest symptomatic stages of AD (prodromal AD).^{237,312,329} This suggests that tau propagates outside the medial temporal lobe already in the preclinical, presymptomatic phases of the disease, in agreement with previous models based on neuropathological data.^{51,83} Data from several studies have suggested that tau deposition in the temporal lobe is related to markers of neurodegeneration and early cognitive deficit (i.e. episodic memory impairment),^{237,246,315,329,333} with this relationships becoming stronger when neurodegenerative changes become more prevalent.³³⁴ Based on these observations, it is conceivable that there is a lag phase between the build-up of tau pathology and the development of neurodegeneration, where the deposition of tau precedes the changes in markers of neurodegeneration and cognitive impairment. Although it is difficult to infer the temporal relationship between A β and tau depositions based on the current observations, the existence of A β -positive, cognitively normal volunteers with relatively low levels of tau in the lateral temporal lobe indicates that the spreading of tau pathology outside the medial temporal areas follows in time the cortical accumulation of fibrillar A β .²³¹ Overall, we suggest that tau pathology spreads early in the lateral areas of the temporal cortex before the onset of neurodegenerative changes and cognitive deficits, but after the cortical accumulation of A β plaques (Figure 26). Based on earlier evidence for other biomarkers,²⁸⁶ we hypothesised a sigmoid-shaped curve for depicting the temporal course of tau pathology. Furthermore, it is likely, based on neuropathology data and early *in vivo* evidence,^{49,233,234} that the proposed time course could be shift leftward or rightward on the time axis to better depict the earlier deposition of tau in the medial temporal lobe or the later spread in isocortical areas outside the temporal lobe, respectively. Future studies adopting a multi-modal design across the whole spectrum of the disease will improve our understanding of the temporal evolution of tau in the AD brain and offer a chance to validate the proposed model.

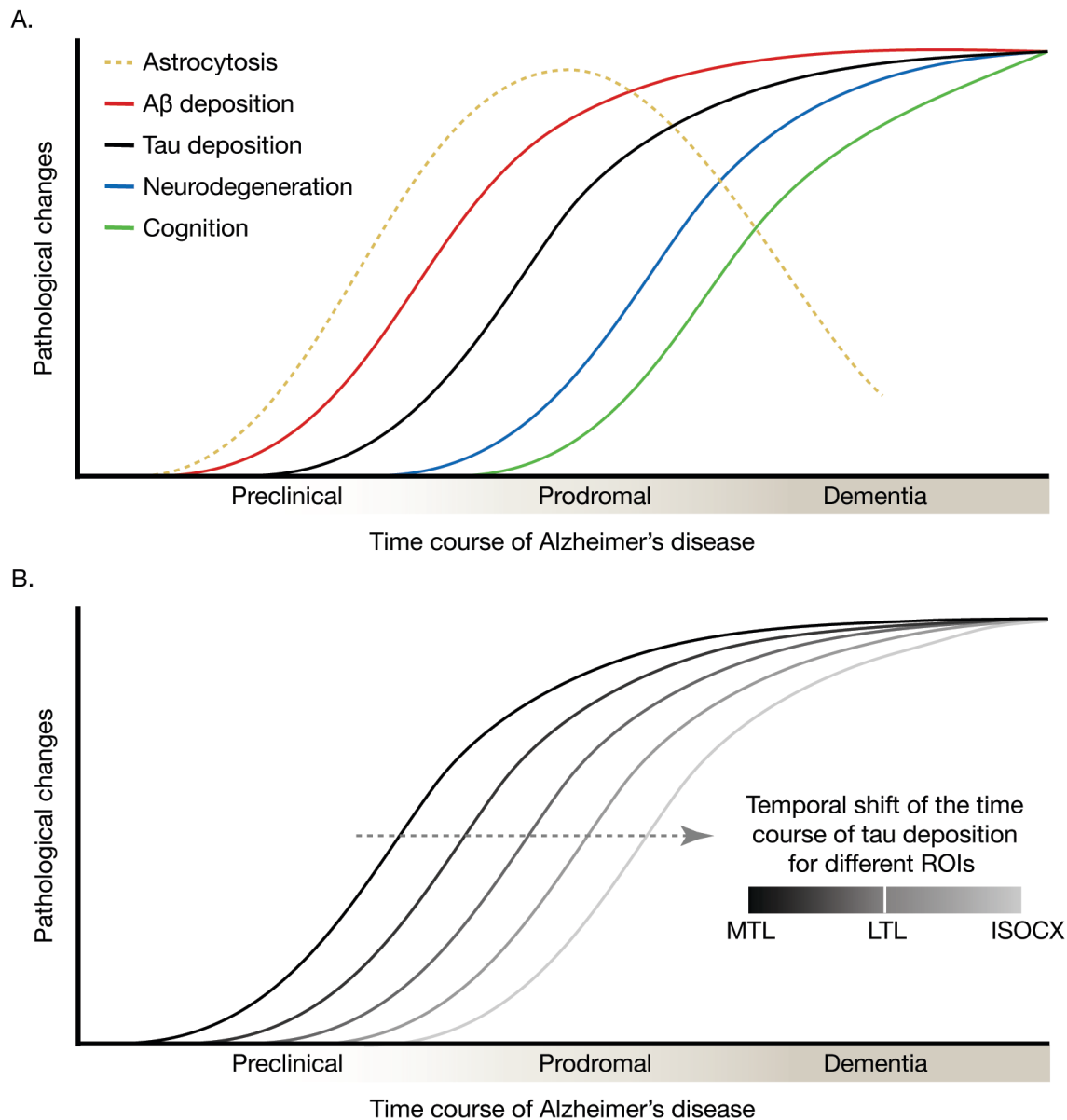


Figure 26. (A) Proposed model of the temporal ordering of the different pathological changes during the development of AD based on biomarker findings for astrocytosis, A β and tau deposition, neurodegeneration and cognitive impairment. (B) Temporal shift of the time course of the build-up of tau deposition for different brain ROIs. ISOCX = isocortex; MTL = medial temporal lobe; LTL = lateral temporal lobe.

7.2 CLINICAL UTILITY OF TAU PET IMAGING

The tau PET tracers have shown promising results at detecting the underlying load of tau pathology in clinically diagnosed AD and non-AD tauopathies that could lead to future breakthrough in the field of tauopathies.^{220,230-232,246-252,329,334} Further research should concentrate on determining whether the different tau PET tracers can discriminate between patients diagnosed with AD or non-AD tauopathies as well as other non-tau-related proteinopathies, based on the load and regional distribution of the tracer binding. This differentiation could lead to great advances in the early, accurate clinical diagnosis, especially in the field of non-AD tauopathies, such as CBD and PSP, where there is, to date, a lack of reliable pathology markers able to be used in the clinic.

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